

A collaborative research to develop a 6 T 230 mm room-temperature bore high temperature superconductor MRI magnet

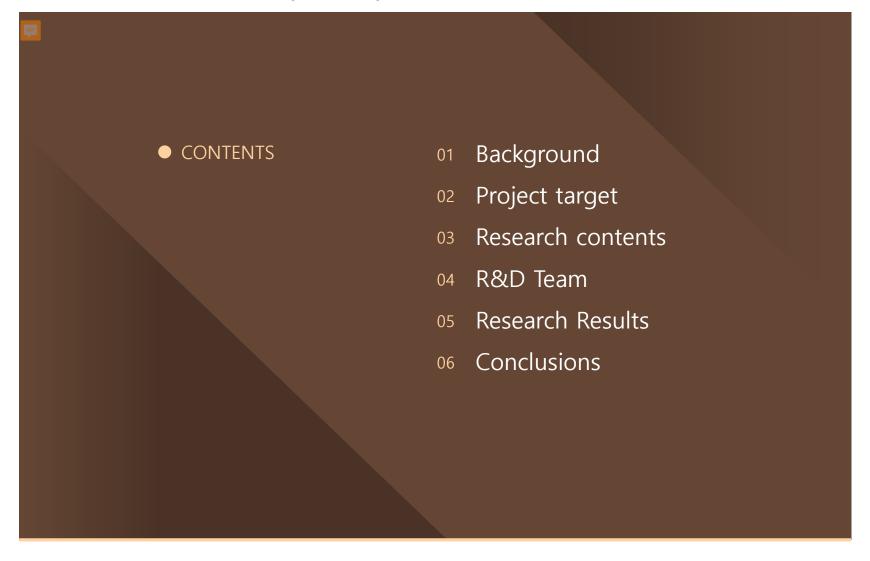
Kideok Sim¹, Seungyong Hahn² and Myung Hwan Sohn³

¹SuperGenics Co., Ltd., ChangWon, Republic of Korea

² Seoul National University, Seoul, Republic of Korea

³ Korea Electrotechnology Research Institute ChangWon, Republic of Korea

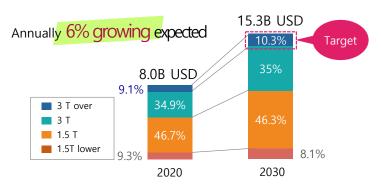
*E-mail: skedy@supergenics.co.kr





1. Background(1)- Why we need higher magnetic field MRI

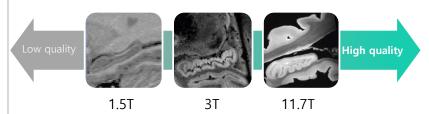
MRI market forecast



MRI market forecast , Future Market Insights, 'MRI Systems Market, Global Industry Analysis

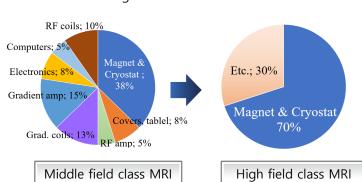
Demand of high resolution MRI

Higher magnetic field magnet provides higher resolution image

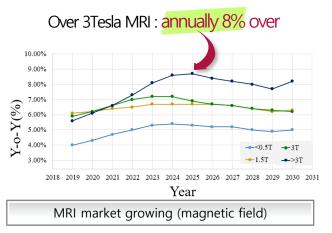


Magnet cost

Medium field 1.5 T class: 38% Ultra high field 7 T over: 70%



High market growing



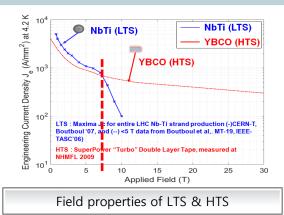
Ref. Future Market Insights, 'MRI Systems Market, Global Industry Analysis



1. Background(2)- Limitation of LTS magnet

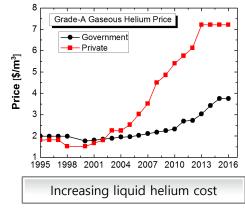
Low temperature superconducting materials limitation

- → Performance degradation under high field applications
- → Low maximum magnetic field
- → HTS materials : better performance at high field

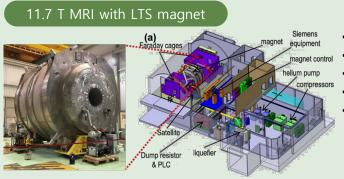


Liquid helium

Helium shortage, cost
→ Expensive operating and maintenance cost



¹REF: U. S. Geological Survey (USGS) Website, Helium Statics and Information, 2017.



- CEA (Europe)
- Size: 4m x 4m
- Weight: 130 ton
- Superfluid helium 1.8K cooling
- Huge space, building requires

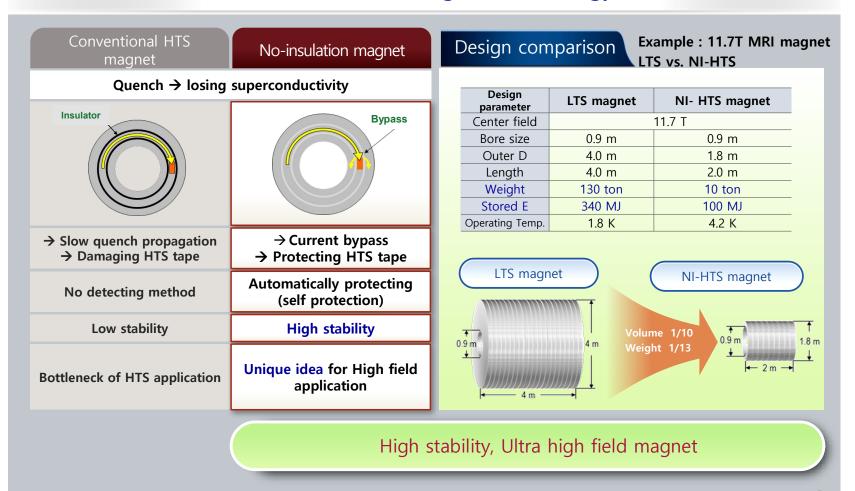
LTS ultra high field MRI

→ Limitation of acceptance to clinical use



1. Background(3)— No insulation HTS magnet

Remove insulation layer: No-insulation magnet technology



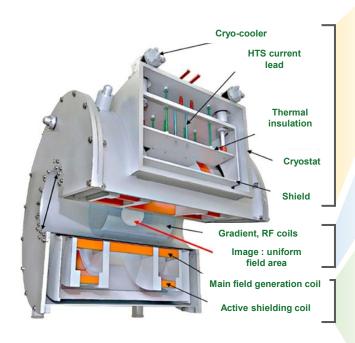


2. Project Target

Sep 2020 ~ Dec 2023 \$3.5M Period (40 months) (Funded by Korea government) SuperGenics Co., Ltd. Collaborators Seoul National University(SNU), Korea Electrotechnology Research Institute(KERI) Kunsan National Univ., ChangWon National Univ., Korea University. Project Target Center field: > 6T Bore: >200mm (RT) Helium free HTS magnet • Central magnetic field > 6T Magnetic field performance · Stable superconducting magnet • RT bore >200mm · Wire supplier : SuNam • Field uniformity: <10 ppm Quench protection · Passive shimming • Distortion by eddy current<10% Conduction cooling• • Field drift : <1ppm/hr · Operating temperature :20K · High performance Gradient coil • Temperature gradient < 5K • Screen current minimize operation Ref: Google Image 'Phillips Helium free MRI system'



3. Research contents— break through technologies



Existing

Small coil conduction cooling

Gyostat manufacturing

HTS current lead

3-axis gradient coil design

Shim coil design/test

RF coil manufacturing

NMR Ferro shimming

High quality magnetic field design

Multi-physics analysis for Electromagnetic&thermal

Quench analysis Magnet protection system

HTS magnet winding technic

Reducing screening current of small scale HTS magnet

Small magnet operation technic

Short time operation test

Upgrade technic through this project

Large magnet conduction cooling

Minimize temperature gradient

Active shielding gradient coil

Gradient coil water cooling

Induced/screen current reducing

RT shim coil design & operation

Ferro shimming technic for high field magnet

High quality, high magnetic field design for HTS MRI

Electromagnetic, thermal and structure stability under high field

Quench protection system design for high field MRI

Developing precise winding technic for HTS tape

Reducing screening current of large scale HTS magnet

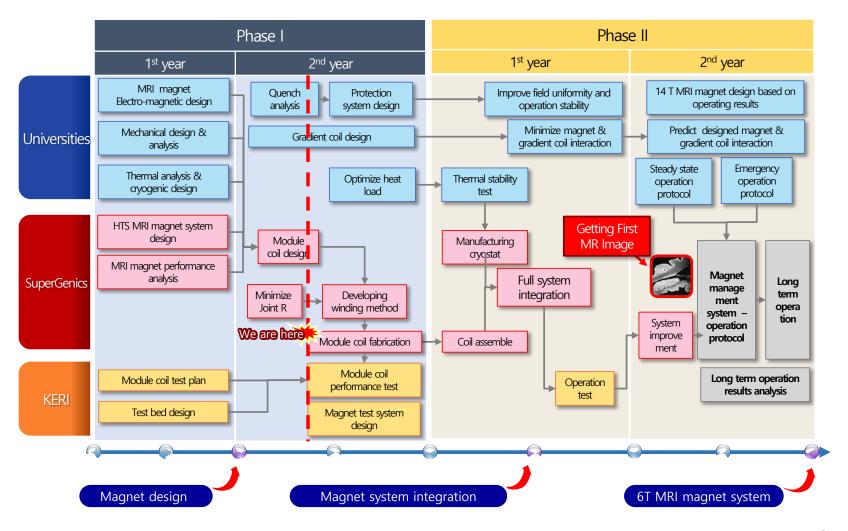
Developing operation protocols for commercial MRI system

Test standard for HTS MRI magnet

Long-time operation reliability

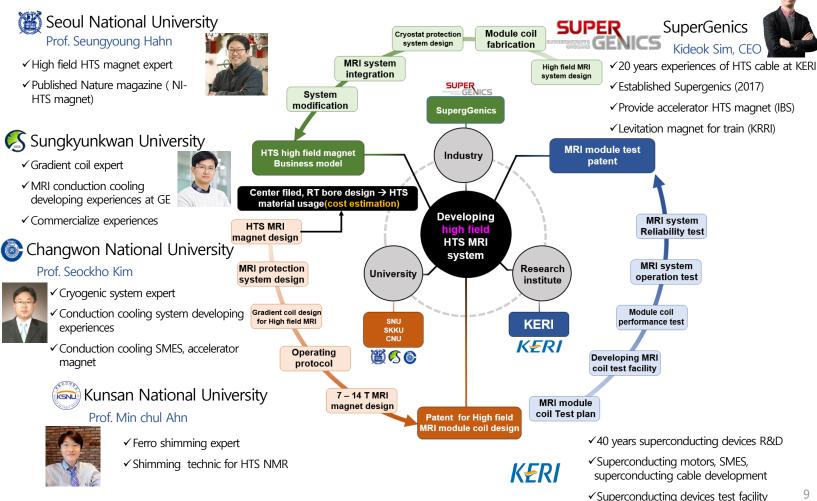


3. Research contents - Road map

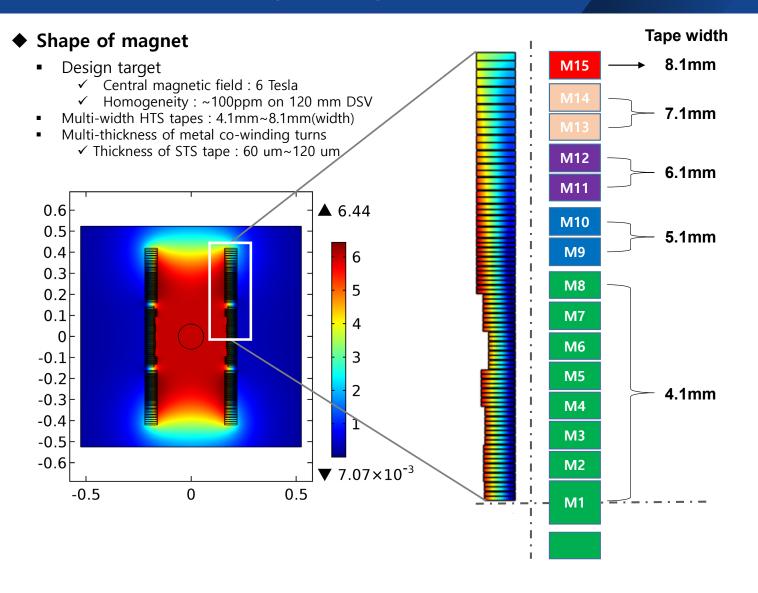




4. R&D Team





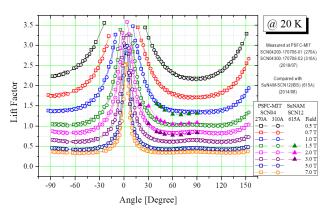


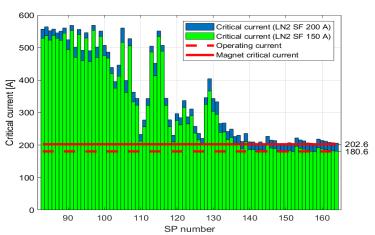


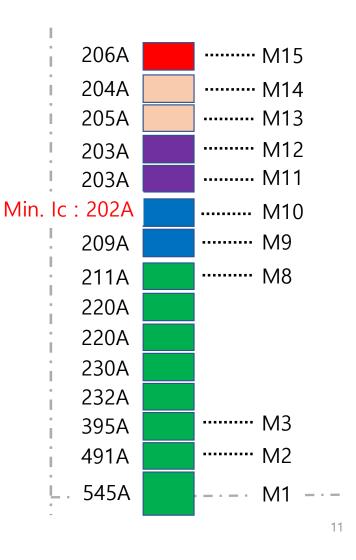
♦ Critical current of magnet

SuNAM HTS tapeIc of HTS tape : 200A @77K SF (4mmW)

• Coil temperature : 20K









Homogeneity of magnetic field

- Ideal design
- **▶** Statistically approach
 - ✓ std error : arise from manufacturing imperfections
 - ✓ Simulated using Monte-Carlo method, assuming standard deviation of tape thicknesses and coil heights are 3 um and 0.2 mm respectively
- Considering SCIF (Screen Current Induced Field) error
 - ✓ Arise from non-linear properties of superconducting resistivity
 - ✓ Simulated using FEM (H-formulation with domain homogenization method)
- Check the change of homogeneity by the thermal contraction after coolong

Harmonics Error of Magnetic Field (120mm DSV) [ppm]							
Order	ldeal design	std error	SCIF error				
1	-	<u>+</u> 84.4	-				
2	-25.6	<u>+</u> 42.5	-70.5				
3	-	<u>+</u> 19.4	-				
4	2.9	<u>+</u> 8.2	-0.4				
5	-	<u>+</u> 3.3	-				
6	-0.2	<u>+</u> 1.3	0				
7	-	±0.5	-				

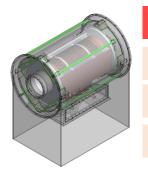


	Paramet	Design Values			
Shape of magnet	Inner radius	s (without bobbin) [mm]	160~173.2 mm		
	Ou	ter radius [mm]	202.72 mm		
	Heigh	nt of magnet [mm]	898.8 mm		
	Number of DPC		82		
Current		op [A] for 6T	180.6		
	I	c [A] (margin)	202.6 (10.9%) @20K		
Magnetic field	B field	(center) [T] @ lop	6		
	Homogeneity (PPM)	Ideal design	28.7		
		Statistically	±313.6 (95% probability)		
		SCIF	70.9		
Energy	Stored energy [MJ] @ lop		1.292		
	Inductance [H]		79.2		



5. Research results – Thermal analysis

♦ Heat load and temperature analysis



Without current

Radiation

Conduction through supports

Conduction through leads



Magnetization loss

Turn-turn current loss

Eddy current loss

Joint and current lead loss

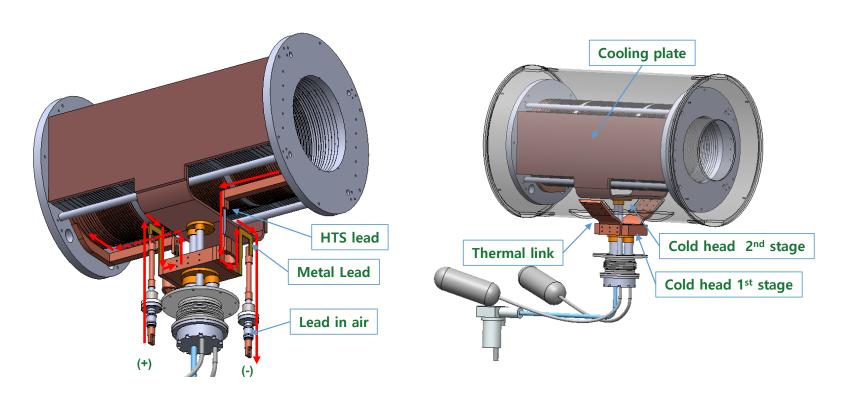


Temperature after Quench

Parts	Heat load [W]				Temperature [K] (min/max/dT)						
	Resist- ance	Radiation	Eddy current	Magneti zation	Turn to turn current	Current leads	Support	Total	w/o Current	with Current	After Quench
Radiation Shield	-	21	-	-	-	25	-	46	-	-	-
Magnet	2.17	0.362	5.55m	1.19	2.67	-	2.65	9.05	10.5 / 11.3 / 0.8	13.6 / 17.0 / 3.4	- / 78.6 / 58.6
Cold head	ead 15.1 W @ 20 K (Cooling capacity of cryocooler, 60 Hz)					10.0	12.3	-			



5. Research results – System design

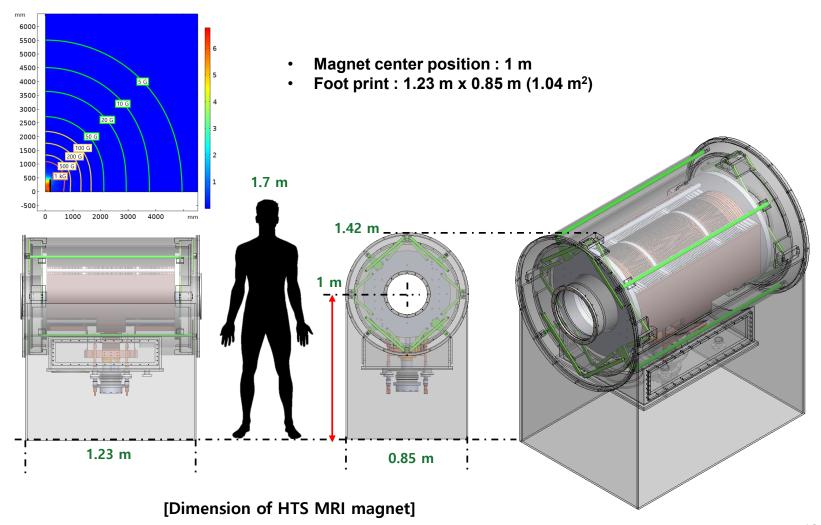


[Current lead of Magnet]

[Cooling path]



5. Research results – System design



6. Conclusion

◆ PLAN

- Due to a limited budget, the magnet room temperature bore size was set to be 230mm. Yet, we are expecting the magnet, once successfully completed, to play an important role as a pilot magnet to fulfill our ultimate goal to develop a next-generation ultrahigh field (>7 T) all-HTS whole-body (>800 mm) MRI magnet.
- After securing magnet performance in this project, we are planning to collaborate with Seoul National University Hospital to use it for the clinical research of infant brain. Furthermore, there is a possibility that our R&D results will be used in the medical device R&D center construction project planned by the local government (KangWon province).

HTS wire

For the development of HTS MRI magnet, high magnetic field wire is important, but a
wire with uniform cross-sectional shape is also important to minimize the effect of
winding errors on the field homogeneity.

CCA 2021 Thank you for Attention!