

# Multichannel on-scalp MEG based on high- $T_c$ SQUID magnetometers

Magneto Encephalo Graphy

Superconducting Quantum  
Interference DevicesDag Winkler<sup>1</sup>Justin F. Schneiderman,<sup>2,3</sup> Alexei Kalabukhov,<sup>1,5</sup>Maxim L. Chukharkin,<sup>1,4</sup> Minshu Xie,<sup>1</sup> Silvia Ruffieux,<sup>1</sup> Christoph Pfeiffer,<sup>1</sup>Thilo Bauch,<sup>1</sup> Edoardo Tralbaldo<sup>1</sup>

- <sup>1</sup> Department of Microtechnology and Nanoscience – MC2, Chalmers University of Technology, Gothenburg, Sweden
- <sup>2</sup> MedTech West
- <sup>3</sup> Institute of Neuroscience and Physiology, SA/GU, Gothenburg, Sweden
- <sup>4</sup> Department of Physics, Moscow State University, Russia
- <sup>5</sup> Skobeltsyn Institute of Nuclear Physics, Moscow State Univ., Moscow, Russia

Knut och Alice  
Wallenbergs  
Stiftelse

## Göteborg at the West Coast of Sweden

The gateway to Scandinavia



# Outline

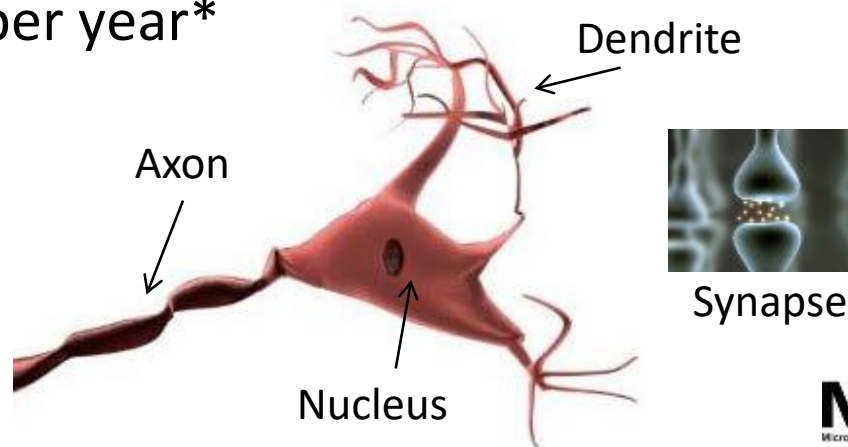
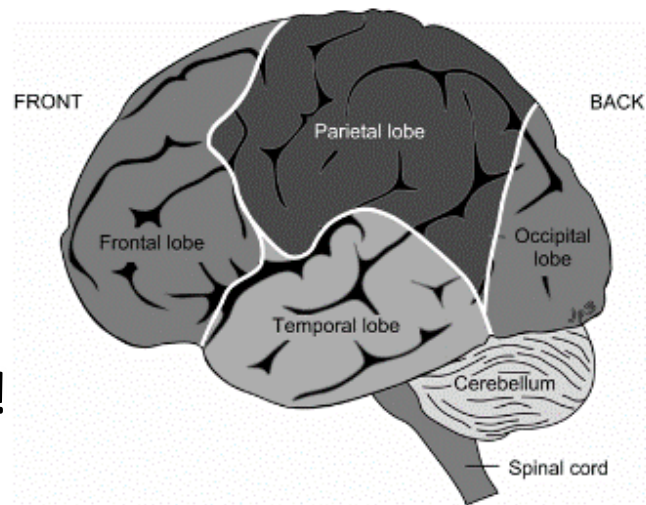
- Introduction
  - Magnetoencephalography (MEG) and focal MEG
  - High- $T_c$  SQUIDs
  - Why high- $T_c$  MEG
- MEG – Benchmarking a single channel high- $T_c$  MEG against a low- $T_c$  ELEKTA MEG
  - Benchmarking experiments with phantoms
  - Benchmarking and protocol for focal MEG on human subjects
- 7-channel high- $T_c$  MEG system (KAW NeuroSQUID project)
  - Direct feedback injection to minimize crosstalk
  - Preliminary measurements
  - Flux transformers
  - High- $T_c$  nanoSQUIDs
    - Single-layer device
    - Flip-chip device
- Conclusion

# Outline

- Introduction
  - Magnetoencephalography (MEG) and focal MEG
  - High- $T_c$  SQUIDs
  - Why high- $T_c$  MEG
- MEG – Benchmarking a single channel high- $T_c$  MEG against a low- $T_c$  ELEKTA MEG
  - Benchmarking experiments with phantoms
  - Benchmarking and protocol for focal MEG on human subjects
- 7-channel high- $T_c$  MEG system (KAW NeuroSQUID project)
  - Direct feedback injection to minimize crosstalk
  - Flux transformers
  - Preliminary measurements
  - High- $T_c$  nanoSQUIDs
    - Single-layer device
    - Flip-chip device
- Conclusion

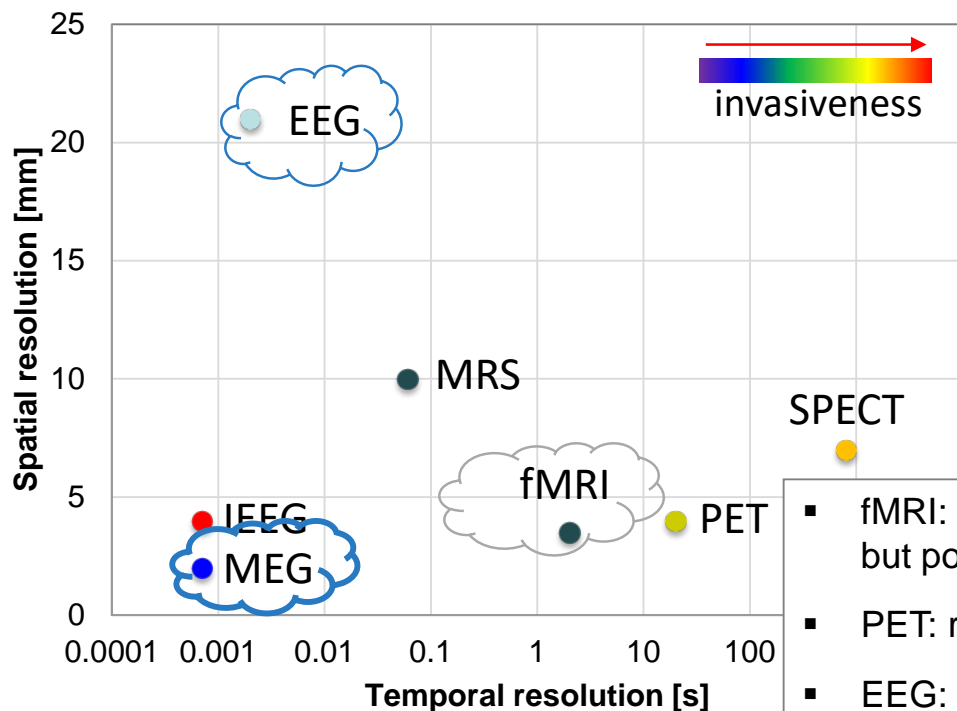
# The human brain

- **Most complex organ known**
  - $\sim 10^{11}$  neurons and  $\sim 10^{15}$  synapses
  - The number of combinations exceeds the number of particles in the universe!
- **Cognition and consciousness**
  - Understanding the brain
  - Philosophical questions
- **Brain disorders a major burden for the society**
  - In Europe, direct and indirect expenses of brain disorders about 800 billion euros per year\*
  - Human suffering



\*) Olesen et al., 2012

# How to interrogate the brain



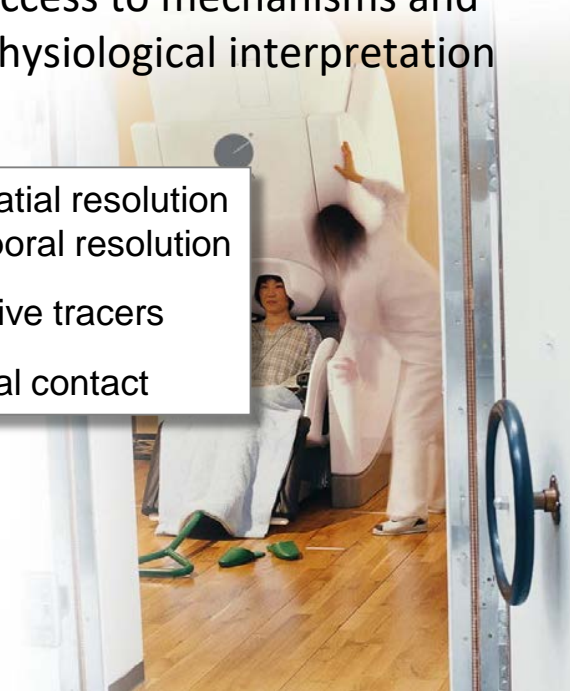
## Benefits of MEG:

- Passive and safe, especially important for infants
- High temporal resolution of ~ms
- Reasonable spatial resolution of ~mm
- Spectral content of the signals
- Access to mechanisms and physiological interpretation

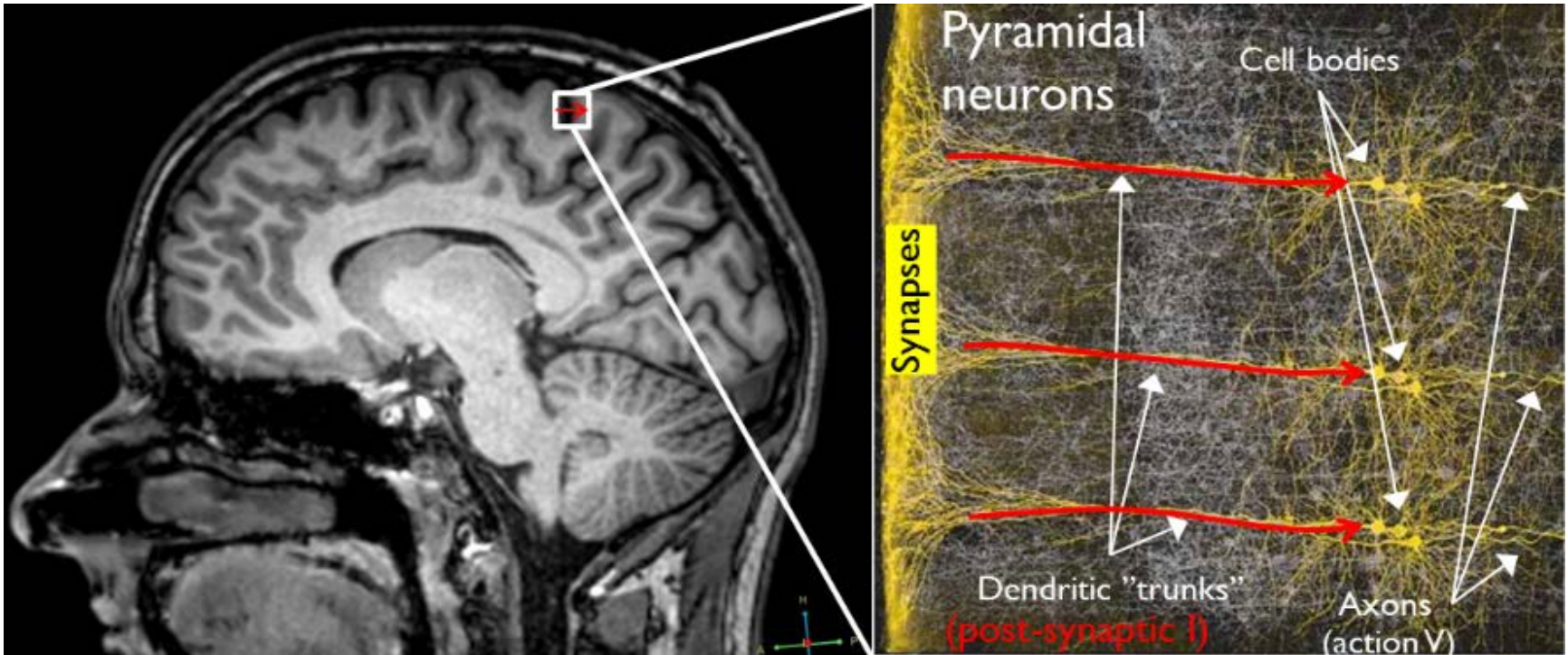
- fMRI: high spatial resolution but poor temporal resolution
- PET: radioactive tracers
- EEG: electrical contact

EEG: Electro-encephalography  
IEEG: Invasive Electroencephalography  
MEG: Magnetoencephalography  
MRS: Magnetic Resonance Spectroscopy

fMRI: functional MRI  
SPECT: Single Photon Emission Cranial Tomography  
PET: Positron Emission Tomography



# The Brain



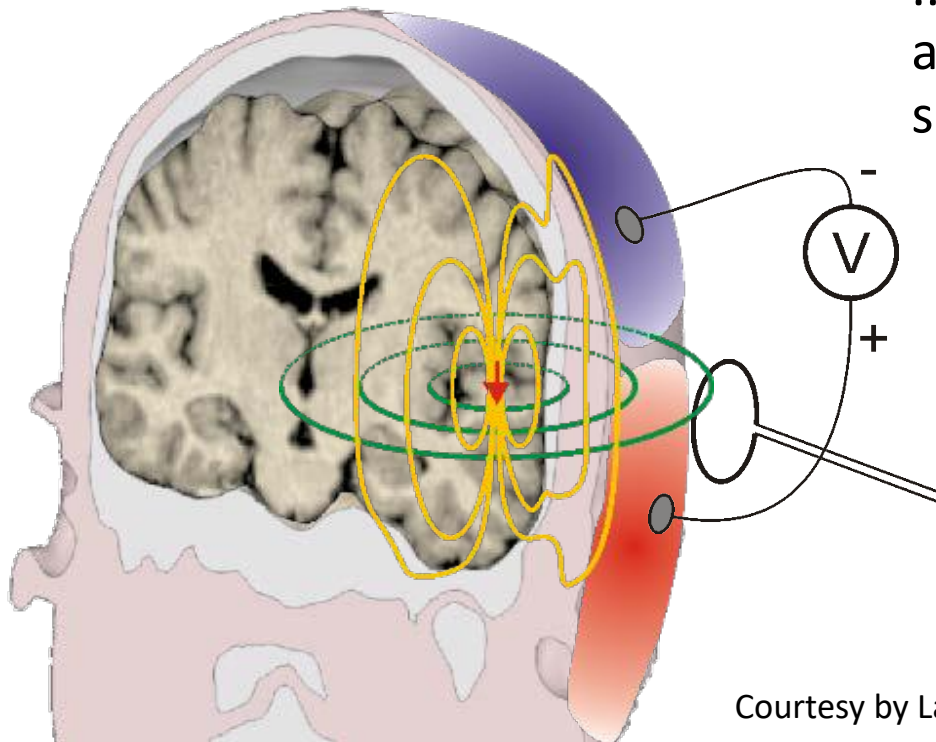
# Magneto- and electroencephalography (MEG/EEG) – measuring electric brain activity

A single neuron:  $B \sim 0.01$  fT

10 000 synchronous and  
parallel neurons:  $B \sim 100$  fT

Currents in **active**  
neurons...

... give rise to small electric voltages  
and weak magnetic fields on the  
surface of the head



EEG = measuring the  
voltages on the scalp

MEG = measuring the  
magnetic fields



# Applications of MEG

- Clinical use
  - Epilepsy diagnostics
  - Localization of eloquent brain regions before resections
- Clinical research (e.g.)
  - Predictive diagnostics of Alzheimer's disease
  - Personalized stroke rehabilitation
  - Assessing brain trauma
- Neuroscientific research

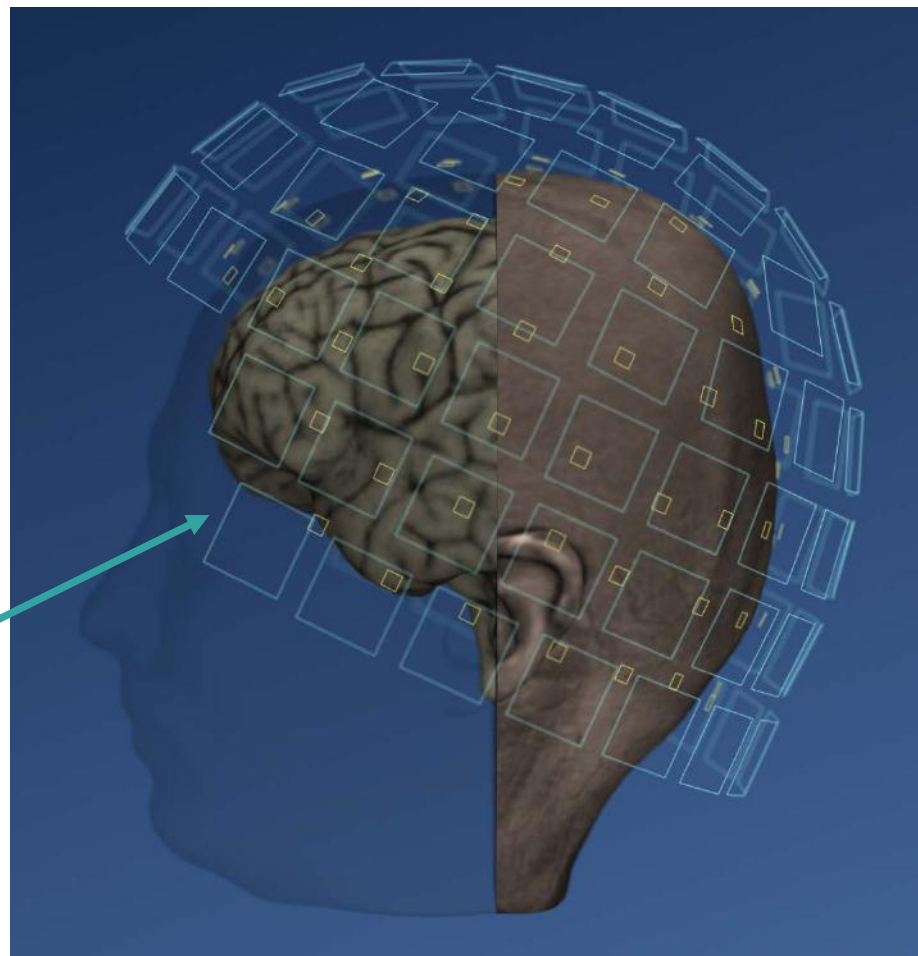
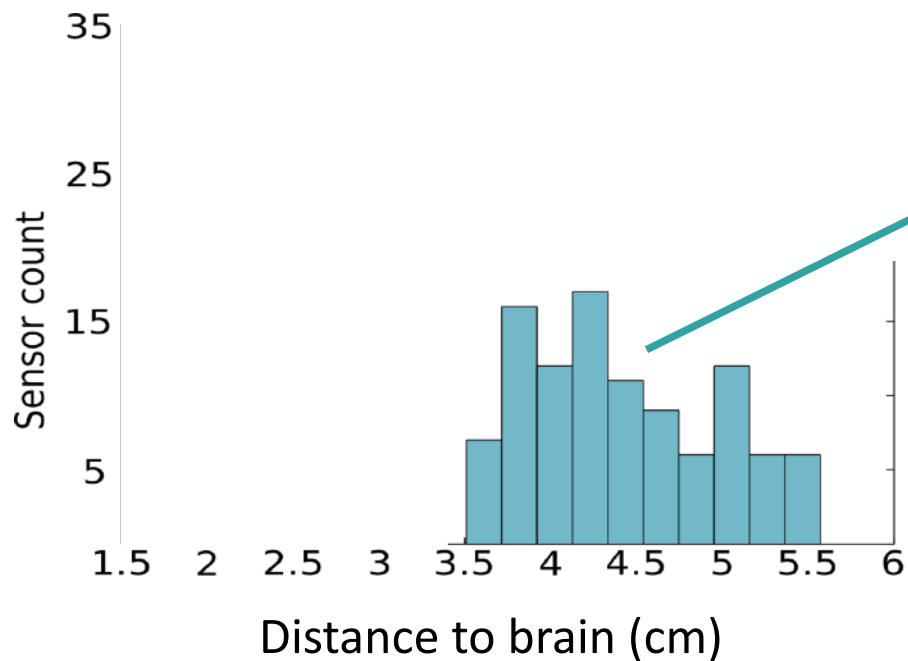
Mäkelä, Paetau & Parkkonen, SUST 2016

Courtesy by Lauri Parkkonen

# Current MEG system's issue: Sensors are far from the brain!

MEG with superconducting LTS-SQUID sensors – LHe cooling:

- ➡ non-adaptable sensor helmet
- ➡ large distance from brain to sensors
- ➡ limited spatial resolution

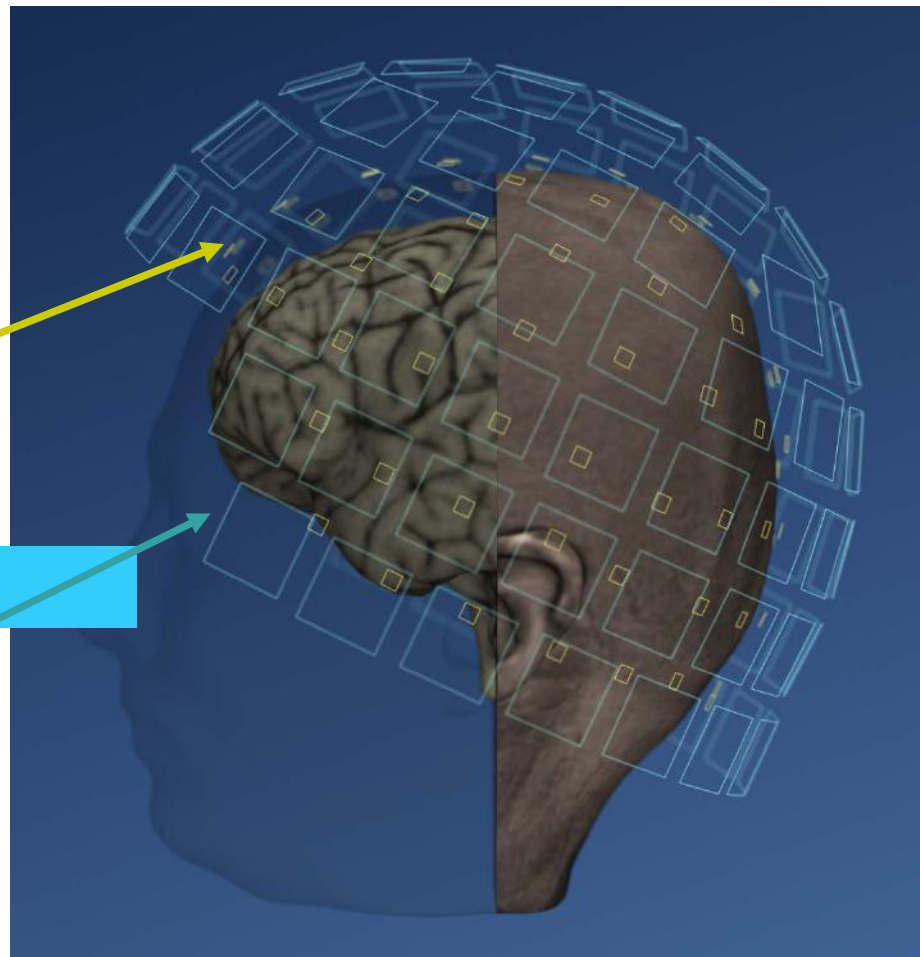
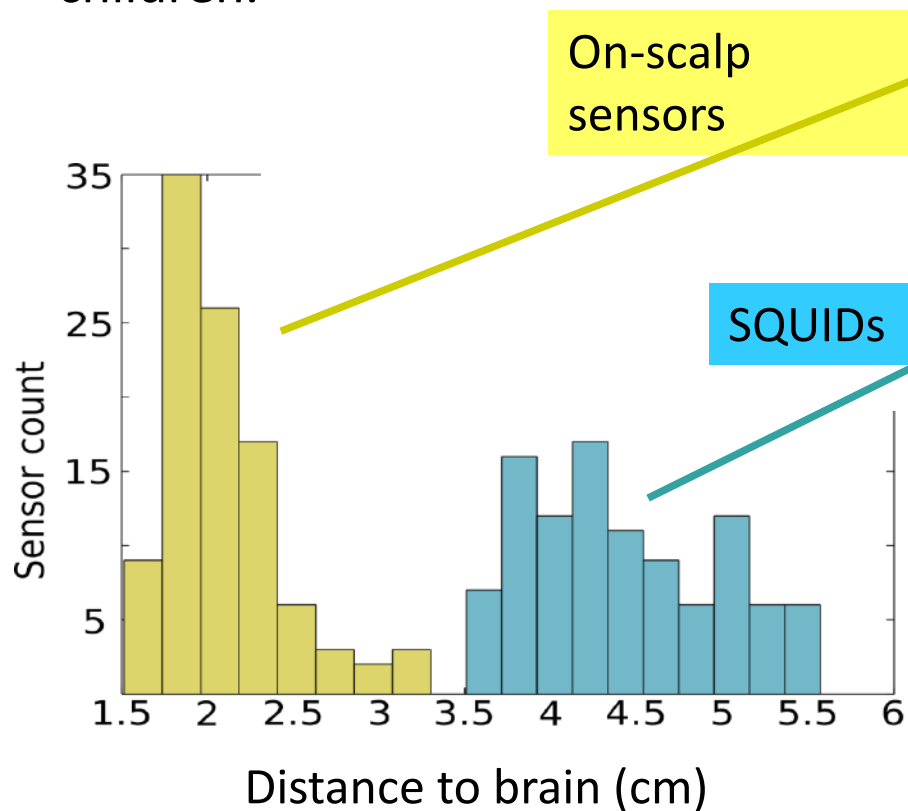


livanainen, Stenroos, Parkkonen (HBM 2013)

Courtesy by Lauri Parkkonen

# If the sensors could be on the scalp...

Distance to brain surface would reduce to less than half in adults. Even larger change in children.



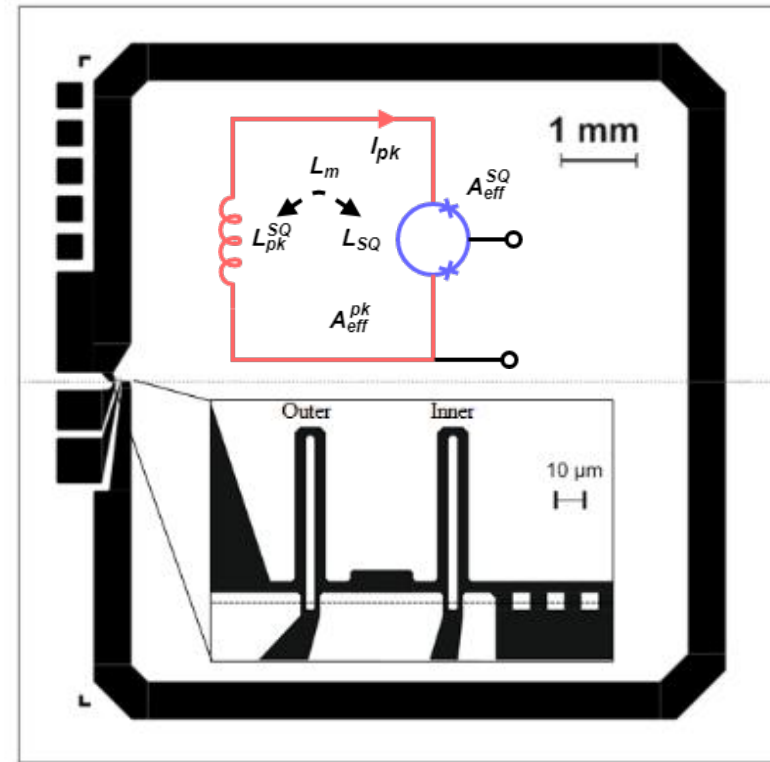
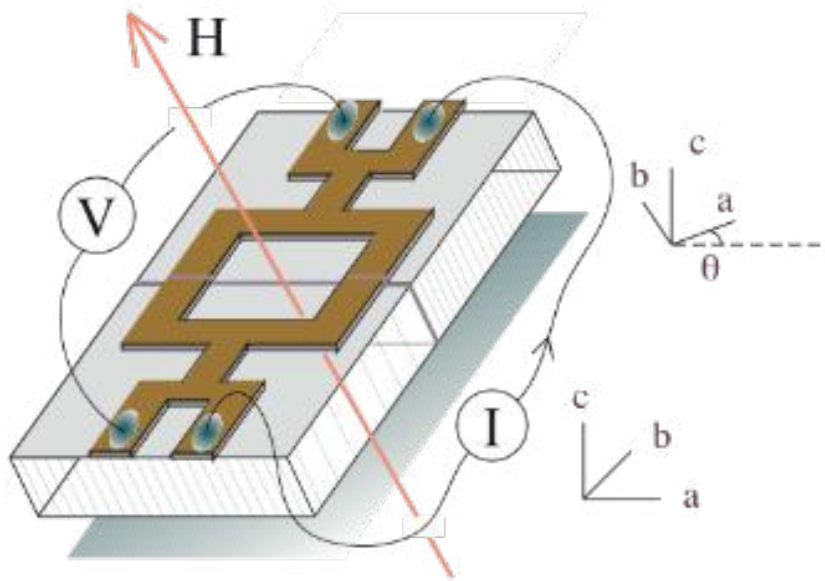
*livanainen, Stenroos, Parkkonen (HBM 2013)*

Courtesy by Lauri Parkkonen

# Why on-scalp MEG?

- Closer to the source
  - Larger signals
  - Can possibly get the same SNR with less sensitive sensors
  - Higher spatial resolution
  - Higher information capacity
  - Resolve more complicated sources?
- Avoid LHe (finite resource, ~500 kSEK/yr)
  - Can use
    - High- $T_c$  SQUIDs at LN2 or
    - (OPMs heated above RT)
  - Simpler cryogenics for high- $T_c$ 
    - Flexible arrays
    - Cheaper systems

# Focal MEG sensors in our case: HTS dc-SQUIDS based on bicrystal junctions

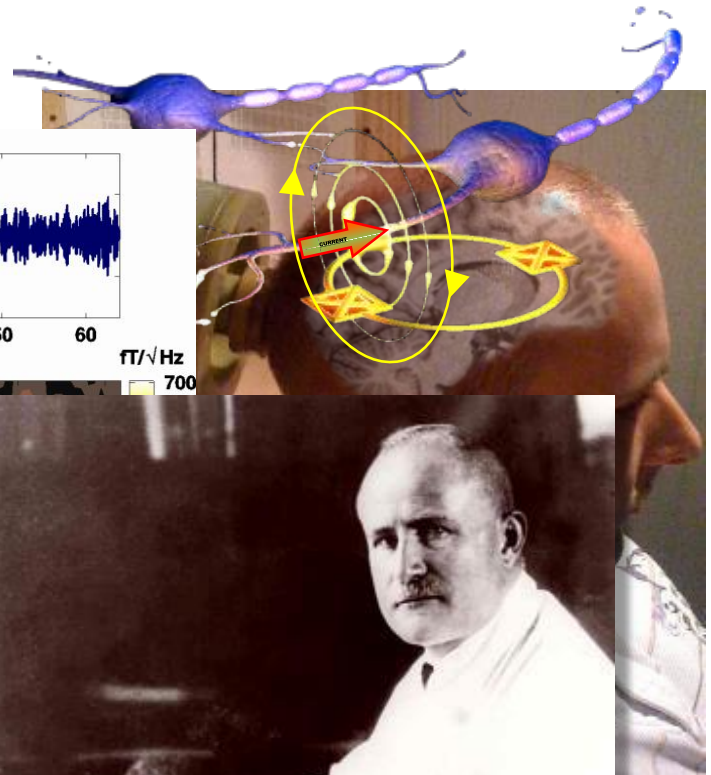
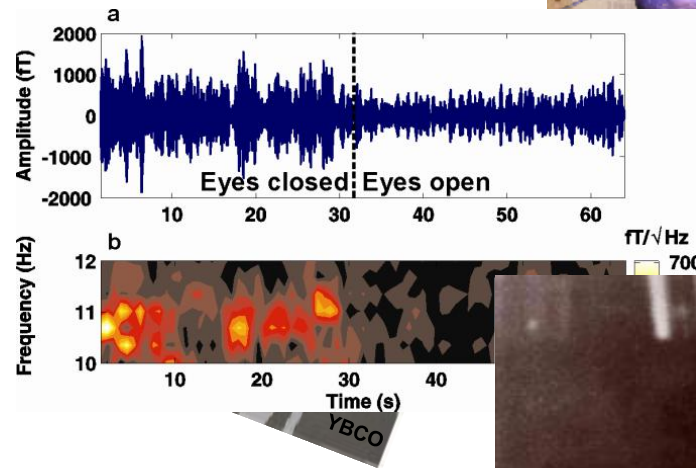


Weak links: bicrystal substrate  $\rightarrow$  grain boundary  $\rightarrow$  epitaxial YBCO film  $\rightarrow$  microbridges crossing the grain boundary

# High- $T_c$ SQUID magnetometers for MEG in an ILK dewar



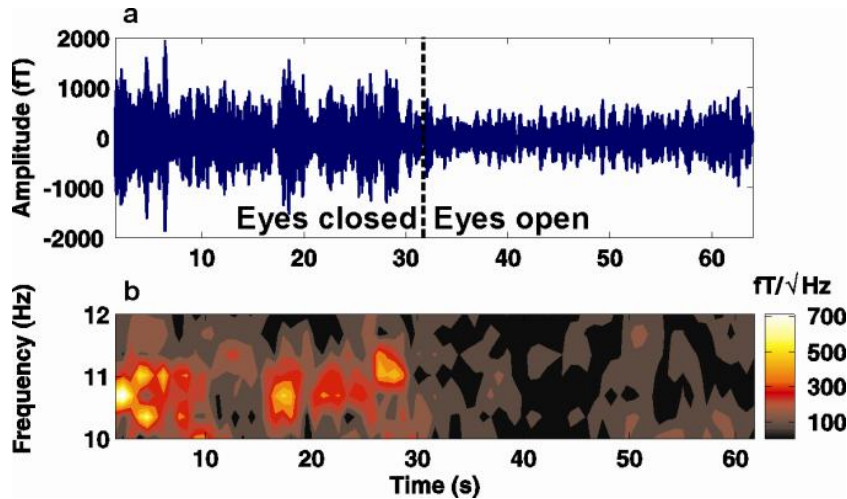
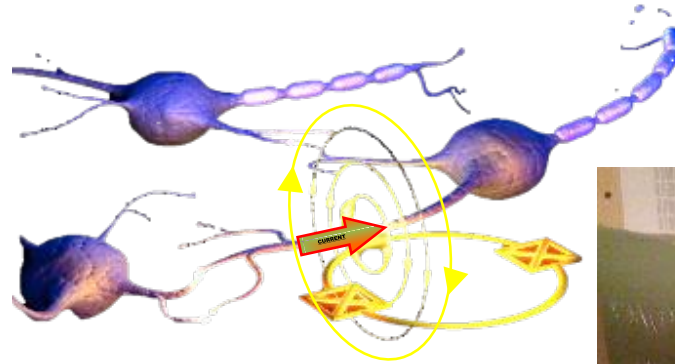
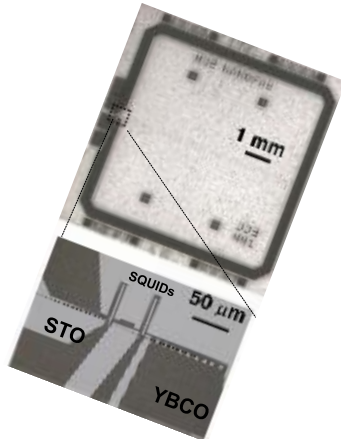
# Graduate student & SQUID & FFT



Berger waves/phenomena

Hans Berger and early EEG recordings from the 1930s

# Graduate student & SQUID & FFT





# EEG recordings from 1930s



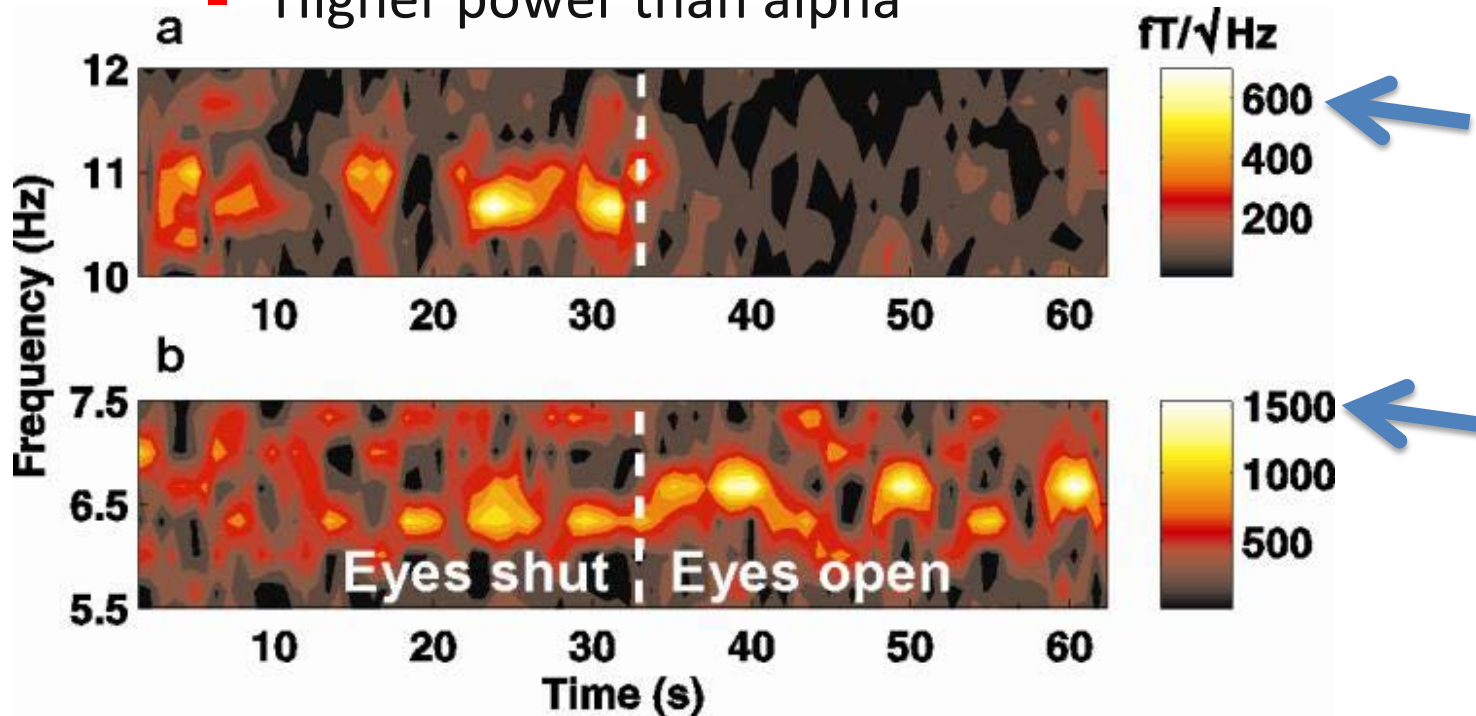
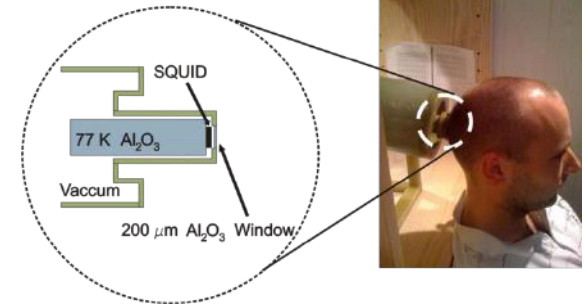
Hans Berger and early EEG recordings from the 1930s

Berger waves/phenomena

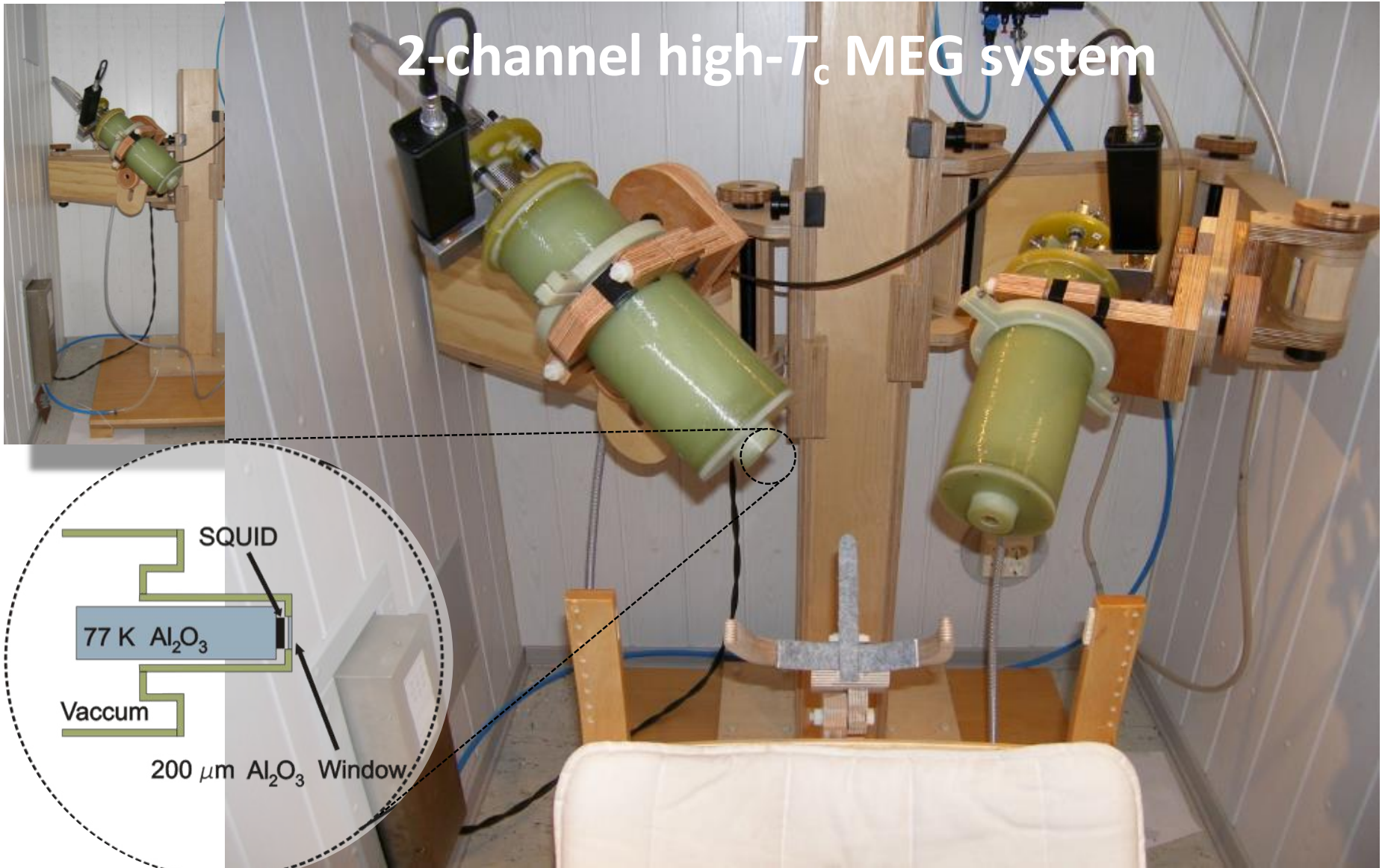
# Alpha and theta bands...

Our first high- $T_c$  SQUID-based MEG recordings

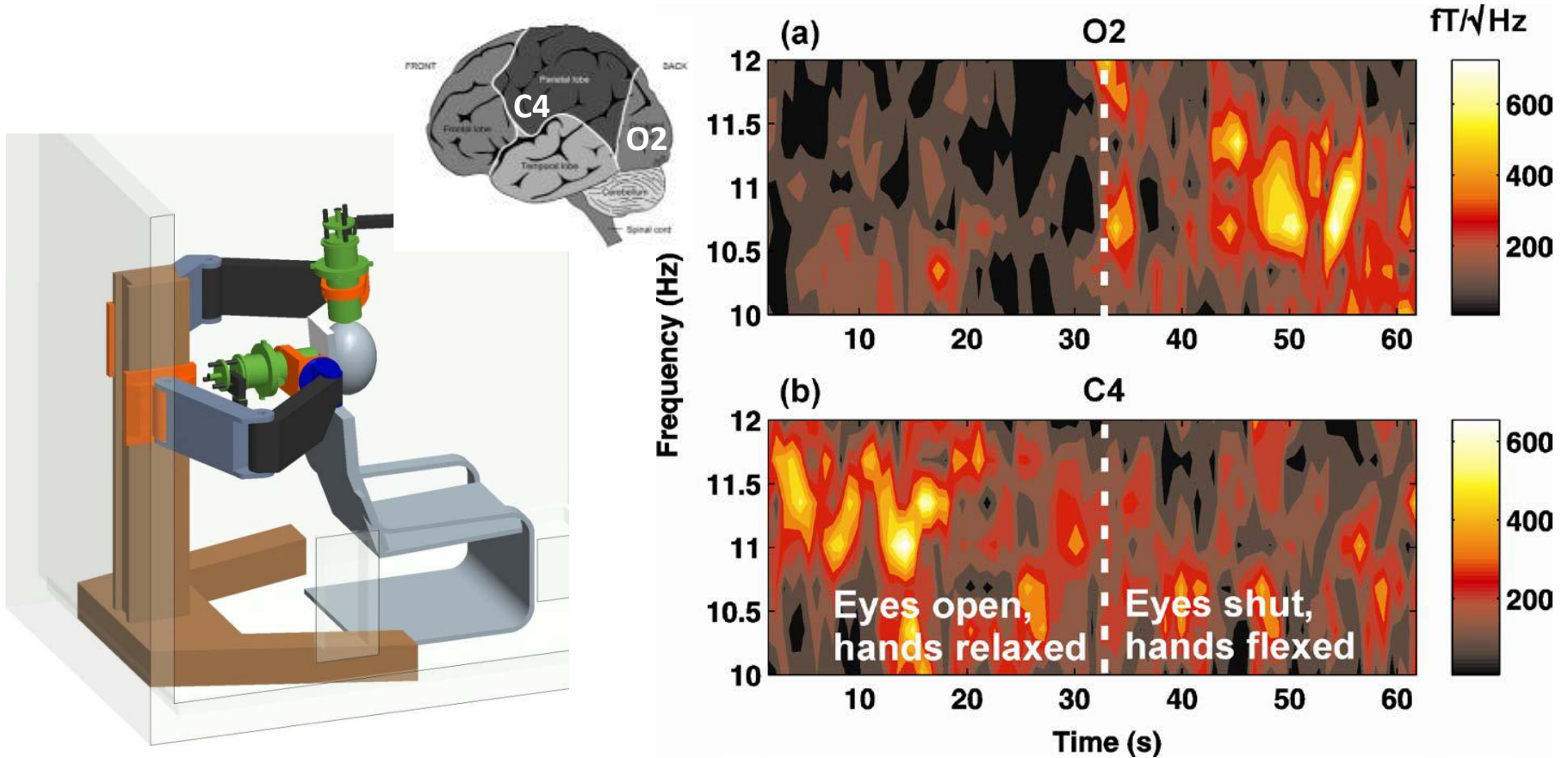
- Alpha modulation as expected
- Something strange in the theta band
  - Atypical of visual system
  - Higher power than alpha



# 2-channel high- $T_c$ MEG system



# Two-channel recordings: visual (O2) and sensorimotor (C4) alpha



Öisjören et al, High-Tc superconducting quantum interference device..., *App. Phys. Lett.* 2012, DOI:10.1063/1.3698152

# Outline

- Introduction
  - Magnetoencephalography (MEG) and focal MEG
  - High- $T_c$  SQUIDs
  - Why high- $T_c$  MEG
- MEG – Benchmarking a single channel high- $T_c$  MEG against a low- $T_c$  ELEKTA MEG
  - Benchmarking experiments with phantoms
  - Benchmarking and protocol for focal MEG on human subjects

1270 IEEE TRANSACTIONS ON BIOMEDICAL ENGINEERING, VOL. 64, NO. 6, JUNE 2017 

## Benchmarking for On-Scalp MEG Sensors

Minshu Xie, Justin F. Schneiderman\*, Maxim L. Chukharkin, Alexei Kalabukhov, Bushra Riaz, Daniel Lundqvist, Stephen Whitmarsh, Matti Hämäläinen, Veikko Jousmäki, Robert Oostenveld, and Dag Winkler

- Single-layer device

- Flip-chip devices
- Conclusion

# Work done in collaboration with **NatMEG @ KI**

Minshu Xie,<sup>1</sup> Justin F. Schneiderman,<sup>2,3</sup> Alexei Kalabukhov,<sup>1,5</sup>  
Maxim L. Chukharkin,<sup>1,4</sup> Silvia Ruffieux,<sup>1</sup> Christoph Pfeiffer,<sup>1</sup>  
Bushra Riaz,<sup>2,3</sup> Daniel Lundqvist,<sup>6</sup> Stephen Whitmarsh,<sup>6</sup> Matti  
Hämäläinen,<sup>7</sup> Veikko Jousmäki,<sup>8</sup> Robert Oostenveld<sup>9</sup>, Dag  
Winkler<sup>1</sup>

- 1) Department of Microtechnology and Nanoscience – MC2, Chalmers University of Technology, Gothenburg, Sweden
- 2) MedTech West
- 3) Institute of Neuroscience and Physiology , SA/GU, Gothenburg, Sweden
- 4) Department of Physics, Moscow State University, Russia
- 5) Skobeltsyn Institute of Nuclear Physics, Moscow State Univ., Moscow, Russia
- 6) Swedish National Facility for Magnetoencephalography (NatMEG), Karolinska Institutet (KI)
- 7) NatMEG, KI and A.A. Martinos Center for Biomedical Imaging, Mass. Gen. Hospital & Aalto Univ.
- 8) NatMEG, KI & Aalto University
- 9) NatMEG, KI & Radboud University



**Karolinska  
Institutet**

**MedTech West**



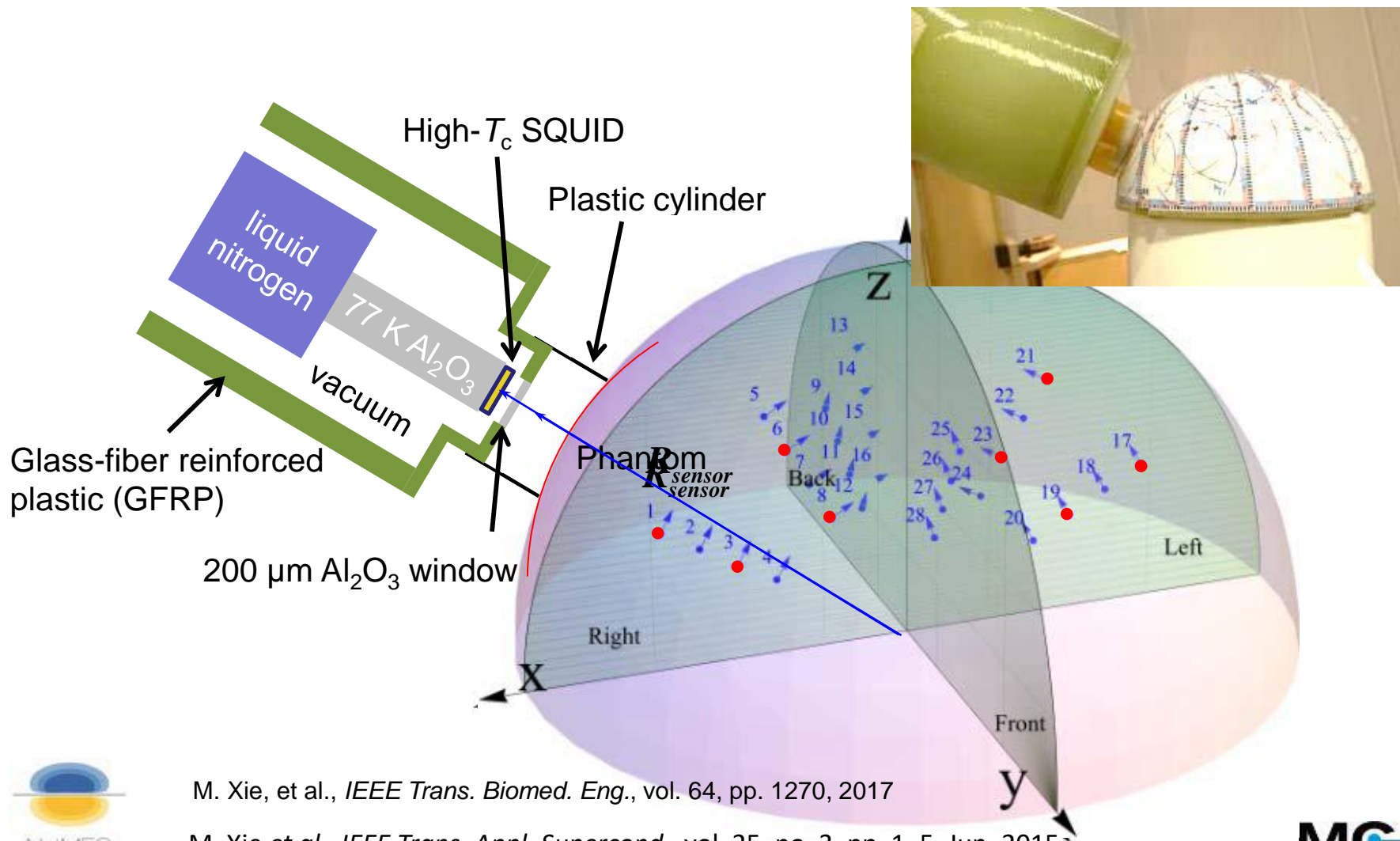
GÖTEBORGS  
UNIVERSITET



CHALMERS

**MC2**  
Microtechnology and Nanoscience

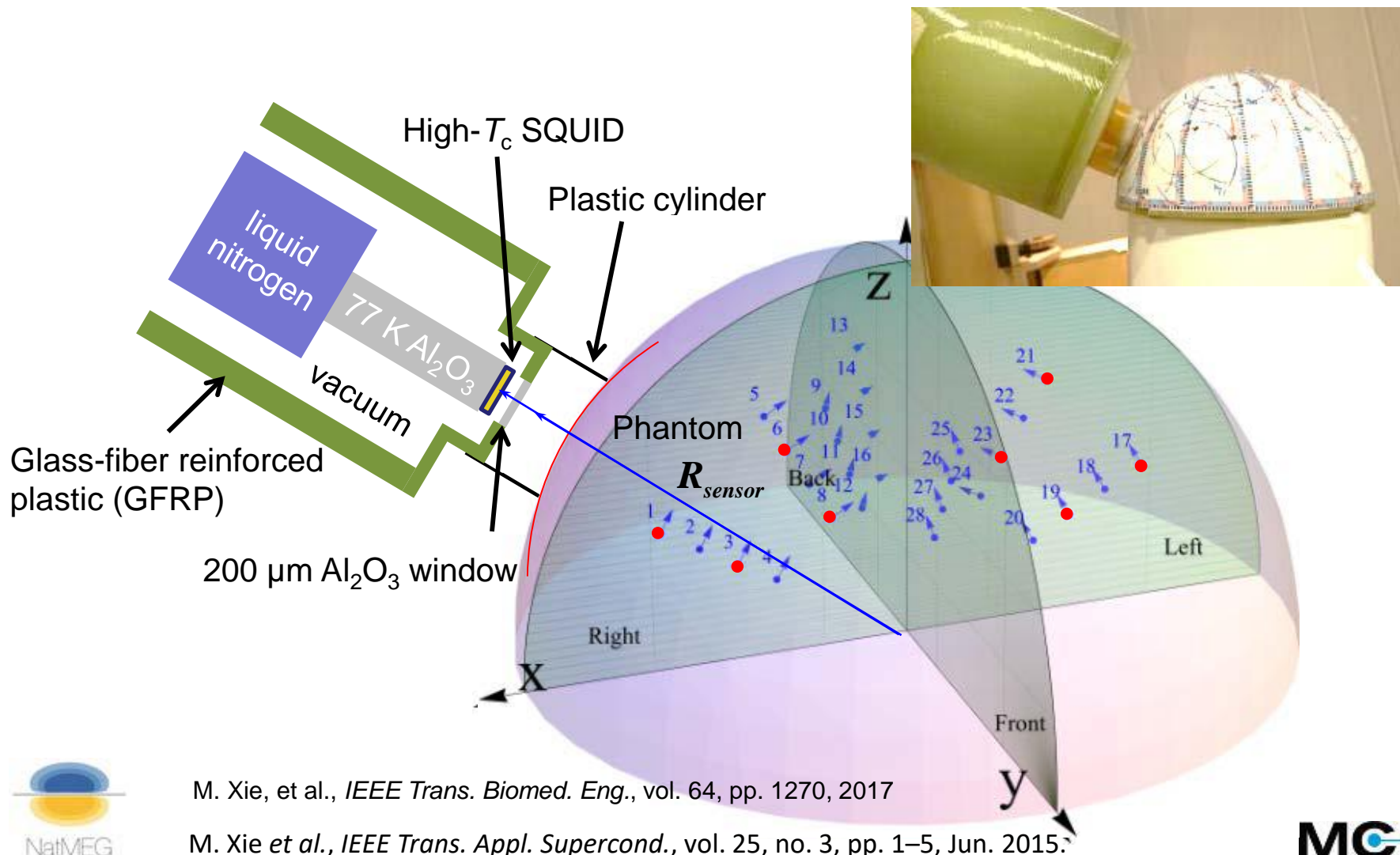
# Benchmarking on phantoms (courtesy of Elekta)



M. Xie, et al., *IEEE Trans. Biomed. Eng.*, vol. 64, pp. 1270, 2017

M. Xie et al., *IEEE Trans. Appl. Supercond.*, vol. 25, no. 3, pp. 1–5, Jun. 2015.

# Benchmarking on phantoms (courtesy of Elekta)



M. Xie, et al., *IEEE Trans. Biomed. Eng.*, vol. 64, pp. 1270, 2017

M. Xie et al., *IEEE Trans. Appl. Supercond.*, vol. 25, no. 3, pp. 1–5, Jun. 2015.

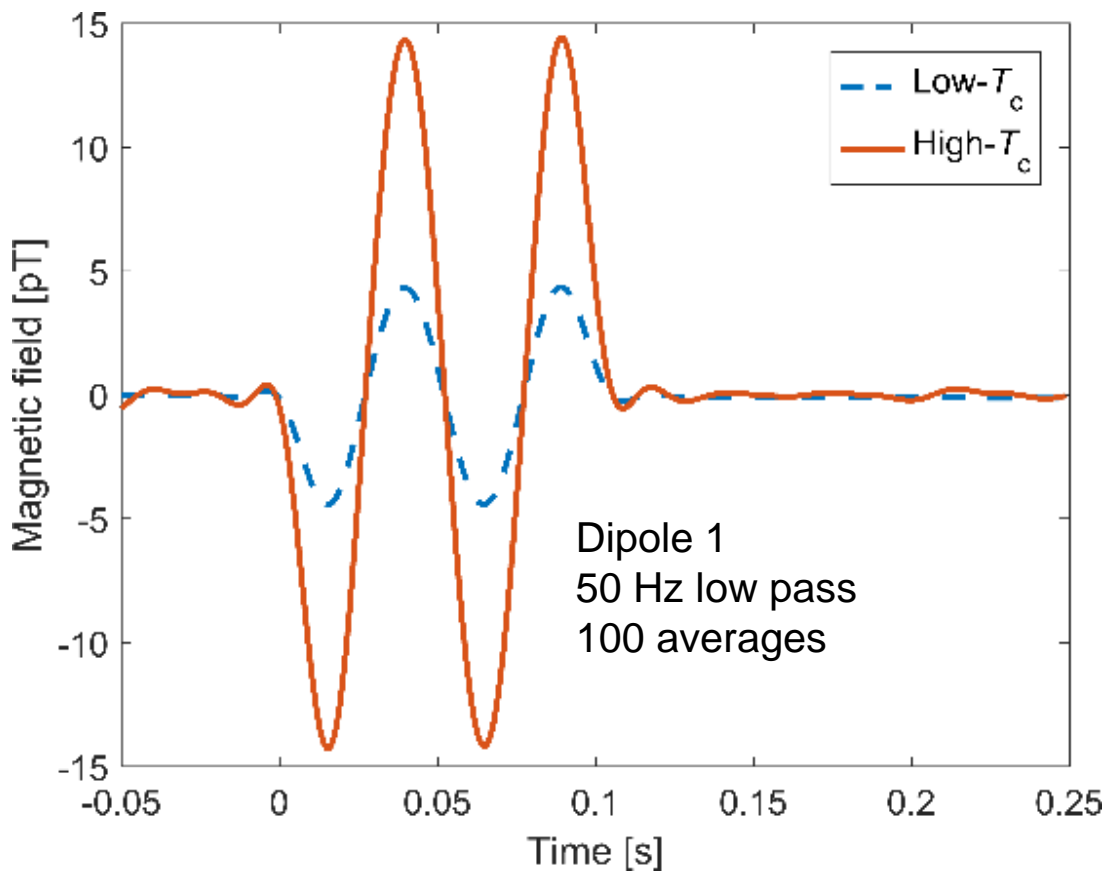


# Results

Standoff distance: 3 mm for high- $T_c$  and 20 mm for low- $T_c$

Dipole 1 depth under the phantom shell: 24 mm

Expected signal amplitude gain: ~3 times



# Benchmarking on human subjects

## Challenges:

**A new benchmarking protocol is needed!**

- The limited number of channels for new sensor technology
- Time consuming to map the full field topography
- Habituation and changes in the subject's alertness during measurement
- The location of sources is unknown - inverse problem needs to be computed!
- To locate the source, full-head field distribution required



# State-of-the-art vs. bicrystal grain boundary high- $T_c$ MEG system

## Elekta Neuromag® TRIUX

102 low- $T_c$  SQUID  
magnetometers and  
204 gradiometers

Capable of full head  
mapping

Sensor-to-subject  
distance **~20 mm**

Sensitivity  
**1–5 fT/√Hz**

Magnetically shielded room  
at KI, Stockholm

## High- $T_c$ MEG system

One or two channels

Single-layer bicrystal  
high- $T_c$  SQUID  
magnetometer

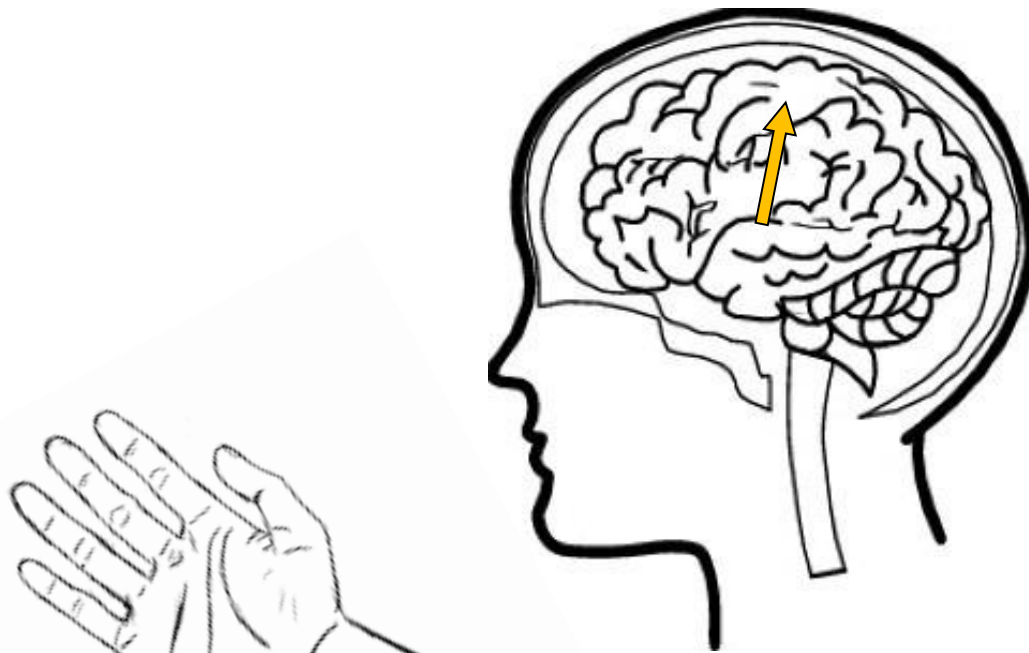
Sensor-to-subject  
distance **~3 mm**

Sensitivity  
**~40 fT/√Hz**

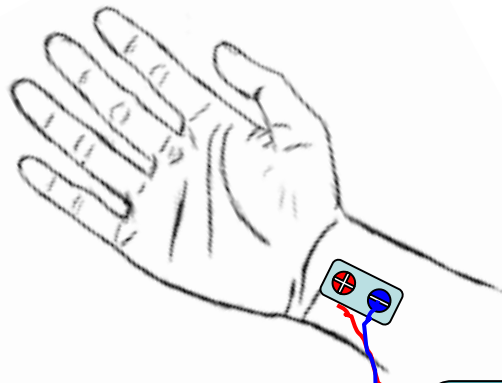


# Benchmarking protocol

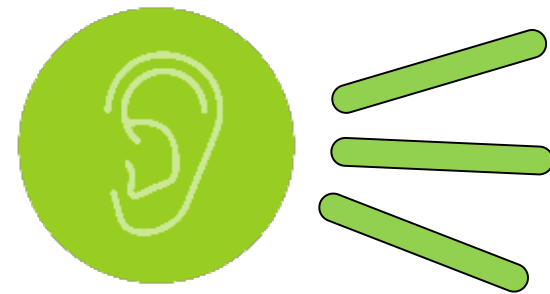
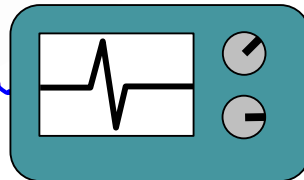
↑ Brain signal



Brain signal



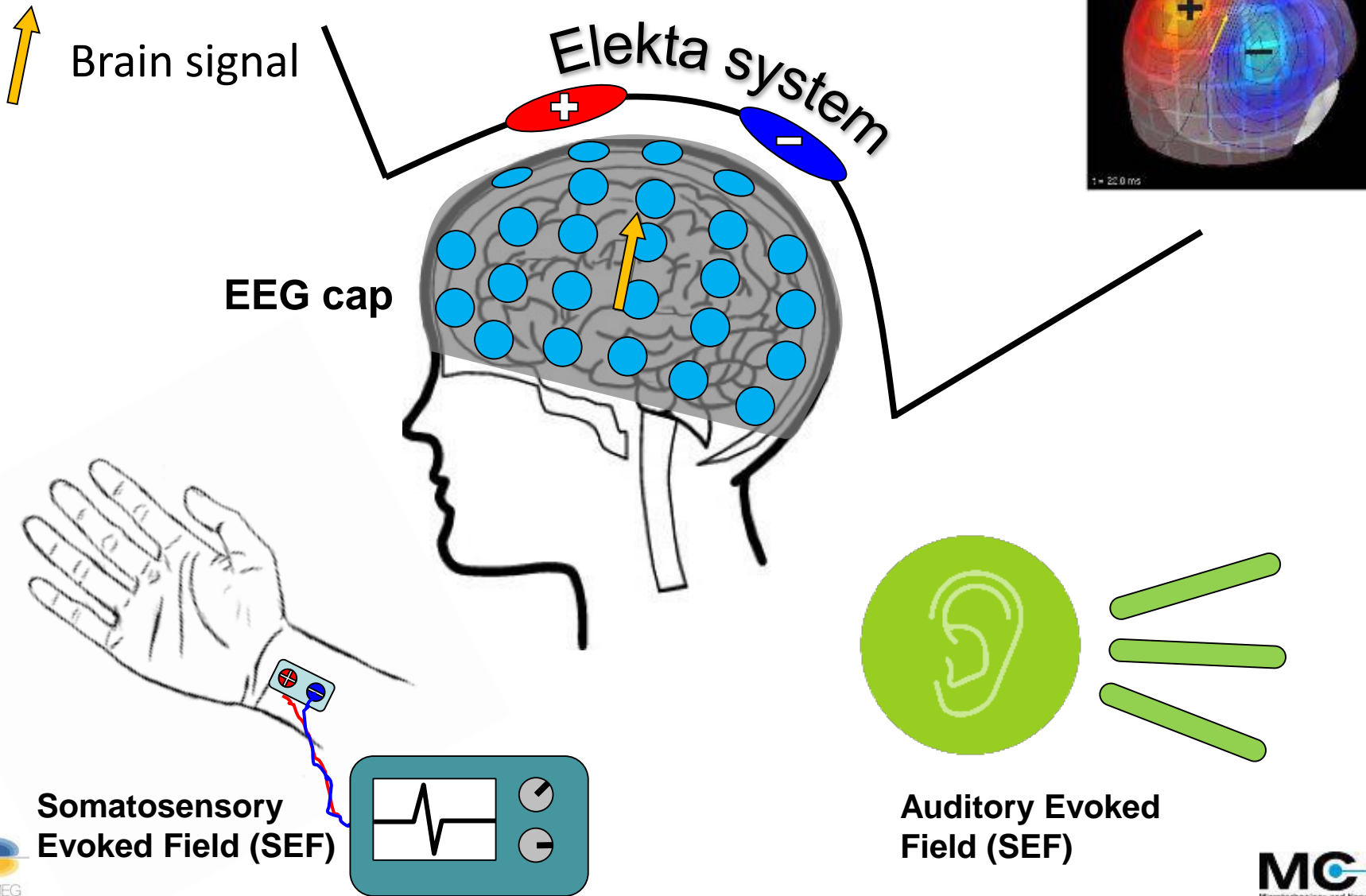
Somatosensory Evoked Field (SEF)



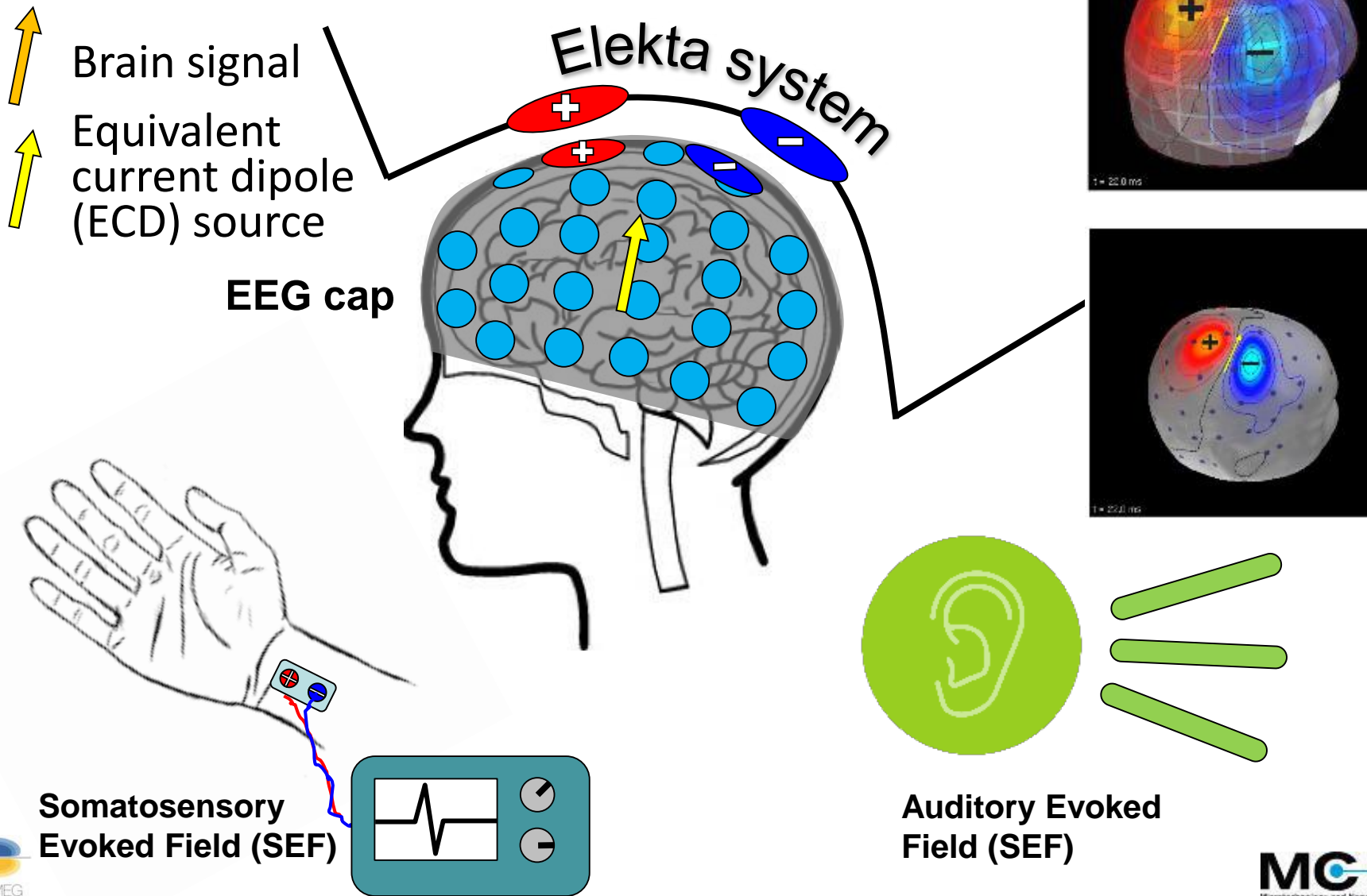
Auditory Evoked Field (SEF)



# Benchmarking protocol



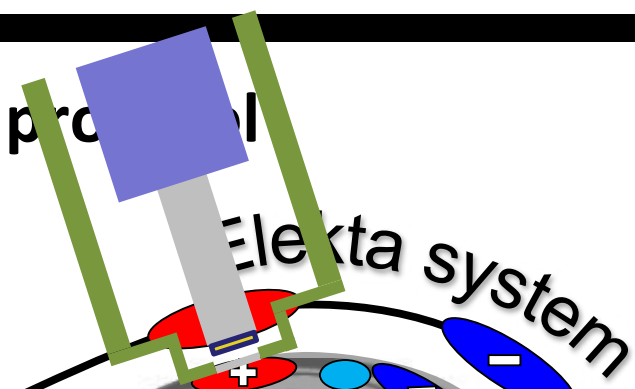
# Benchmarking protocol



# Benchmarking procedure

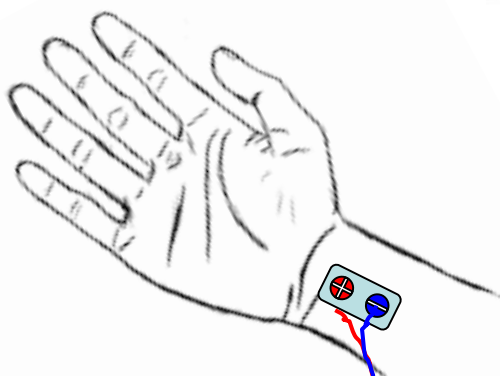
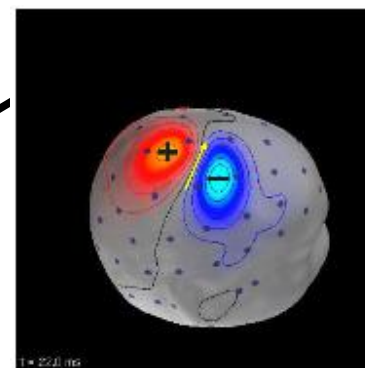
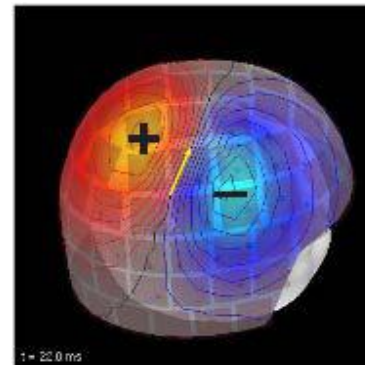
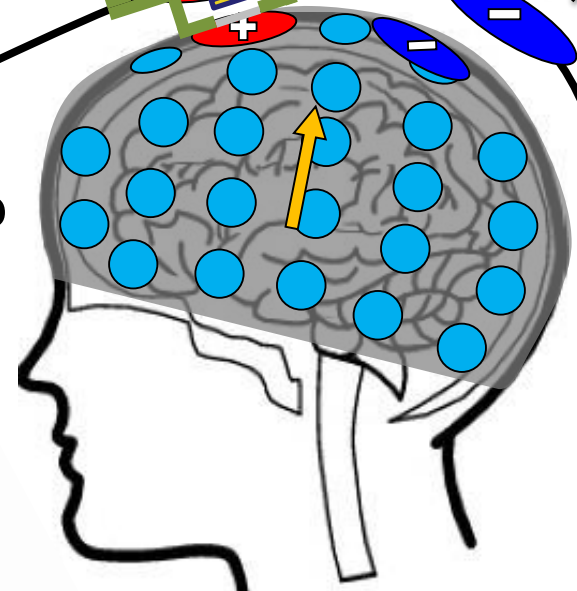


Brain signal

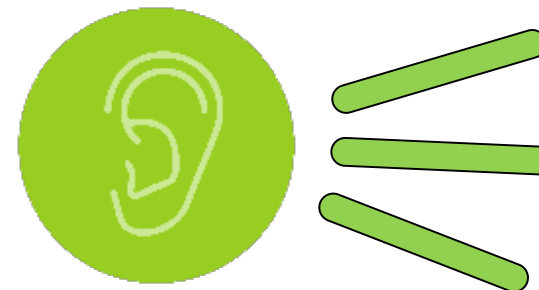


Elekta system

EEG cap



Somatosensory Evoked Field (SEF)



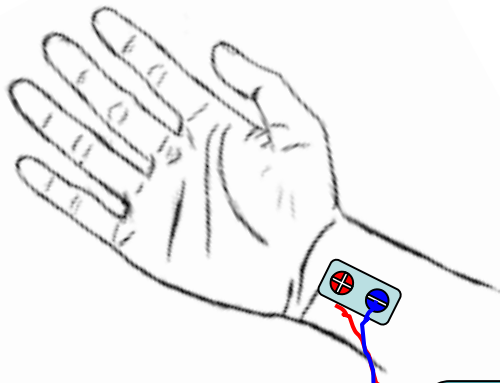
Auditory Evoked Field (SEF)



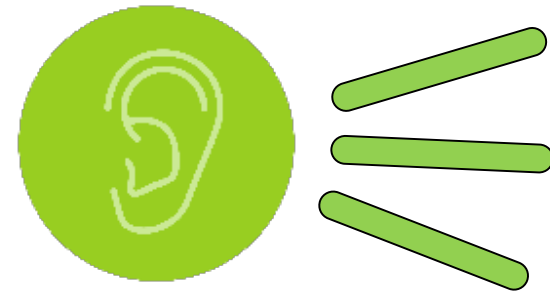
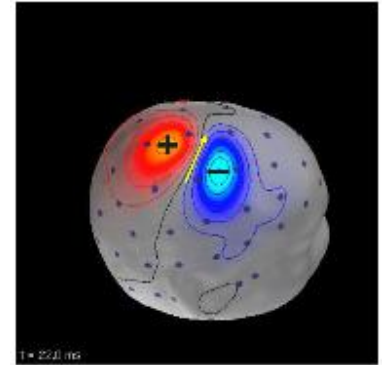
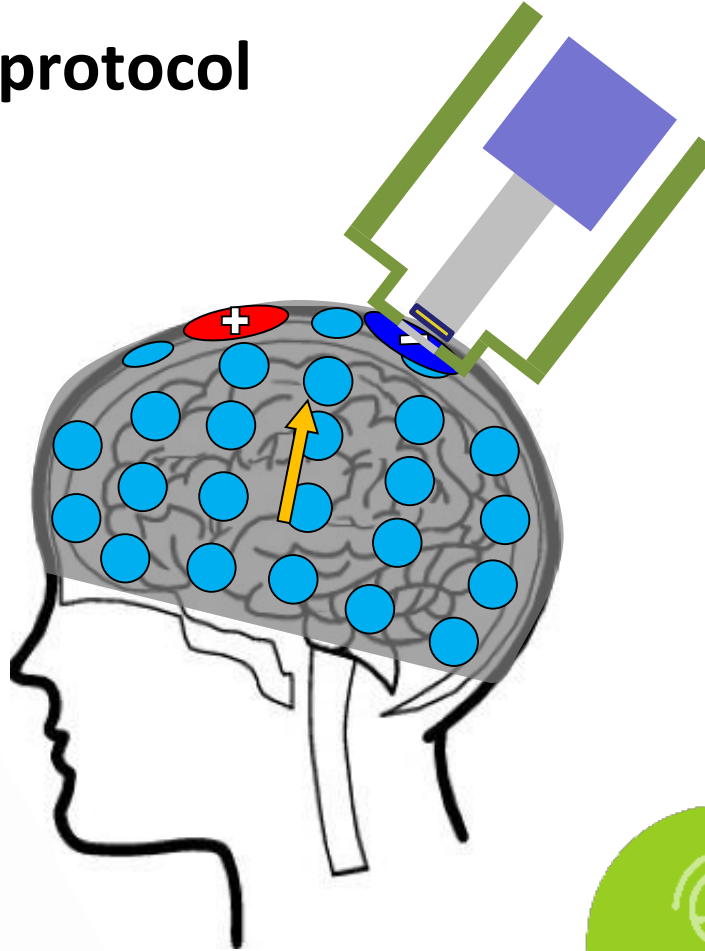
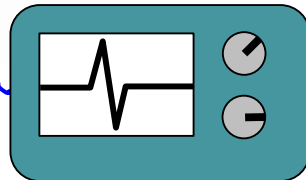
# Benchmarking protocol

↑ Brain signal

EEG cap



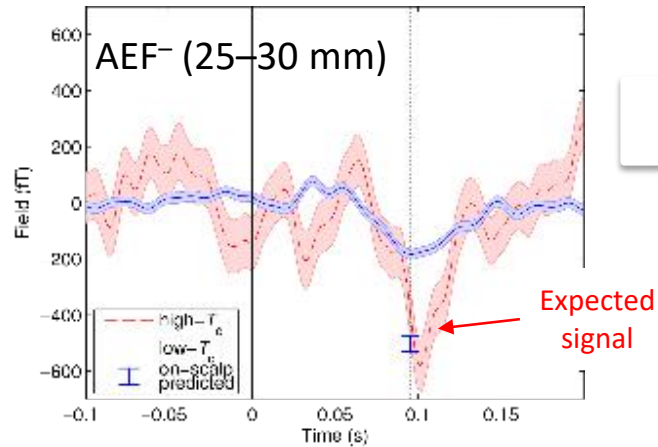
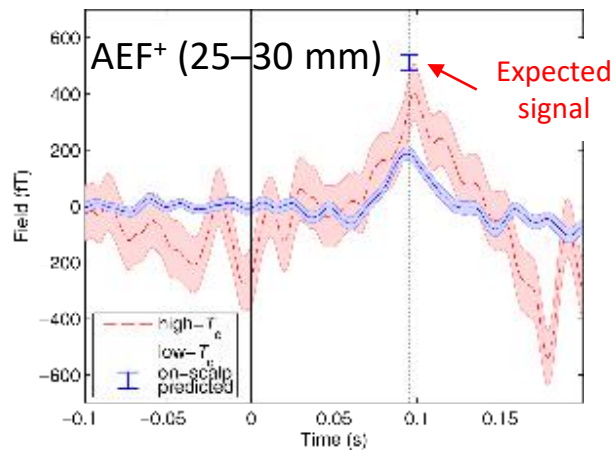
Somatosensory Evoked Field (SEF)



Auditory Evoked Field (SEF)

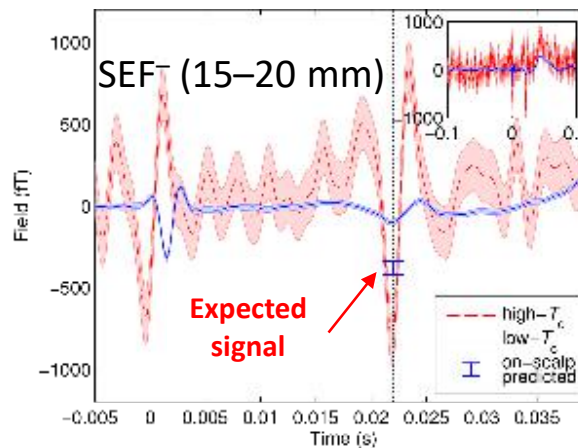
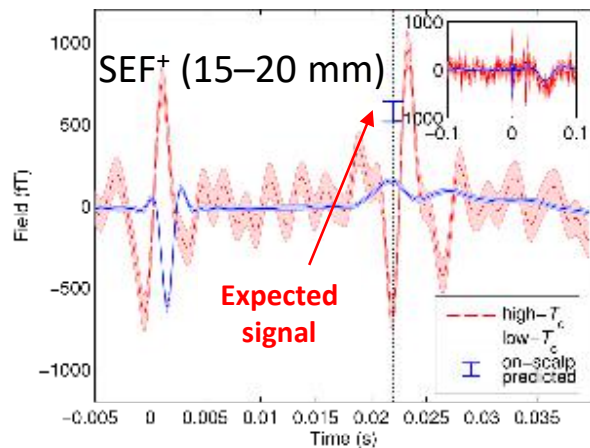


# Results on AEF & SEF



Deep source

Auditory evoked field after ~479 averages and 1-60 Hz band pass filtering



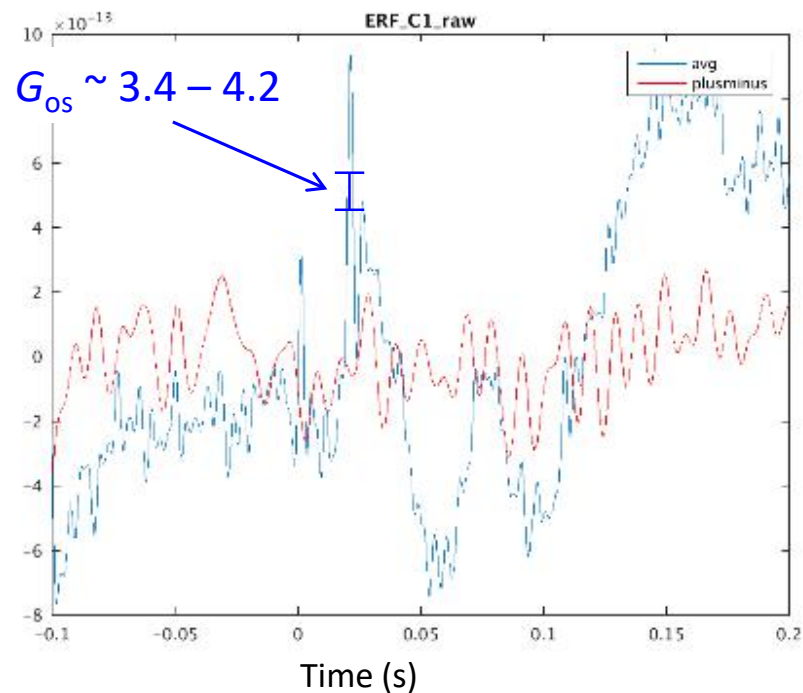
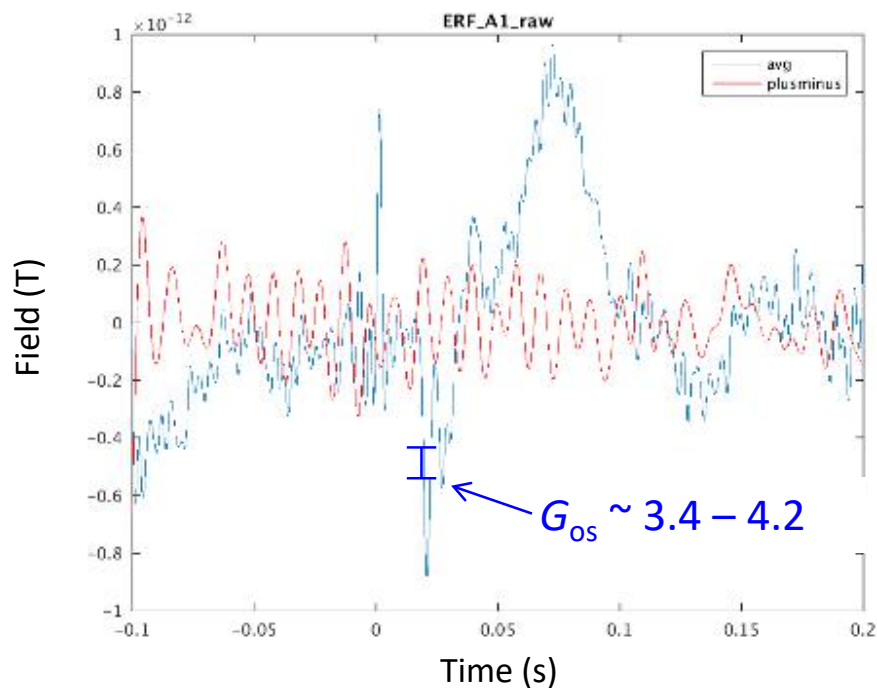
Shallow source

Somatosensory evoked field after ~616 averages and 1-500 Hz band pass filtering  
**More features due to close proximity?** Worth further investigation with on-scalp MEG



# Benchmarking: one high-Tc SQUID vs KI NatMEG Elekta System

- Auditory evoked fields: deep sources, results as expected
- Somatosensory evoked fields: shallow sources, strange results



# Outline

- Introduction
  - Magnetoencephalography (MEG) and focal MEG
  - High- $T_c$  SQUIDs
  - Why high- $T_c$  MEG
- MEG – Benchmarking a single channel high- $T_c$  MEG against a low- $T_c$  ELEKTA MEG
  - Benchmarking experiments with phantoms
  - Benchmarking and protocol for focal MEG on human subjects
- 7-channel high- $T_c$  MEG system (KAW NeuroSQUID project)
  - Direct feedback injection to minimize crosstalk
  - Preliminary measurements
  - Flux transformers
  - High- $T_c$  nanoSQUIDs
    - Single-layer device
    - Flip-chip device
- Conclusion

# NeuroSQUID

## Nanoscale superconducting devices for a closer look at brain activity

*Vision: To make the most sensitive magnetometer capable of operation above 77 K by employing superconducting quantum effects at the nanoscale. Sensors based on this technology will lead to a paradigm shift in neuroimaging. World-leading competences and facilities will come together to explore the fundamental possibilities of this new approach.*

**34 397 000 kronor (~ 4 M\$ / ~460 000 000 JPY)**



**Karolinska  
Institutet**

**MedTech West**



**GÖTEBORGS  
UNIVERSITET**

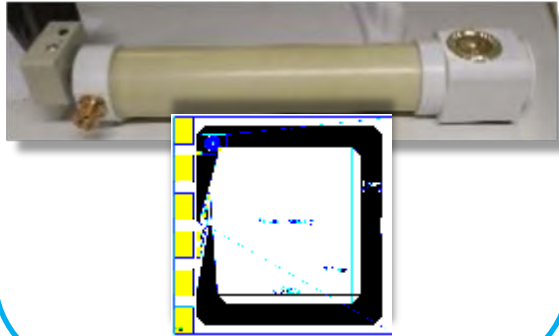


**CHALMERS**

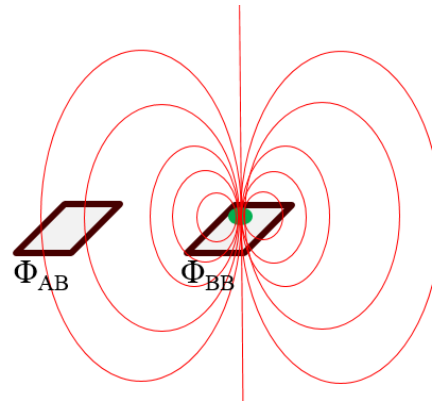
**MC2**  
Microtechnology and Nanoscience

# NeuroSQUID

## Cryostat and sensors



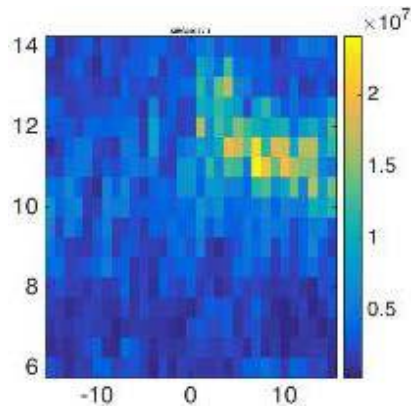
## Crosstalk



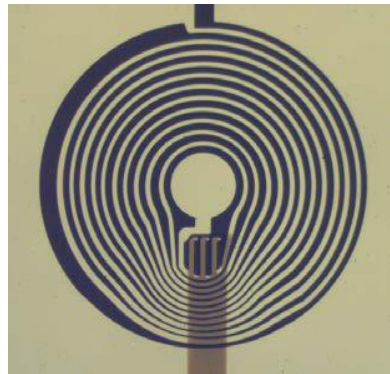
## Head phantom measurements



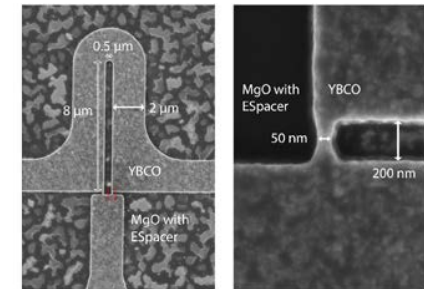
## Preliminary alpha



## Next step: Flux transformers



## Next step: Nanowire-based SQUIDs



# NeuroSQUID

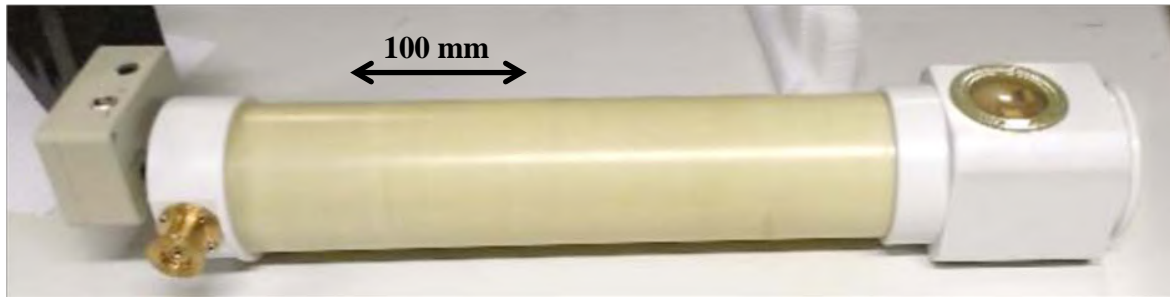
## Cryostat

- 0.9 L liquid nitrogen reservoir
- Vacuum + superinsulation
- Thin, concave plastic window
- Option to pump on nitrogen
- Minimum sensor-to-room temperature distance  $\approx 1$  mm
- $T_{\text{base}} = 80$  K (70 K with pumping)
- $\Delta T < 100$  mK
- $t_{\text{hold}} = 19$  h (22 h with pumping)

# NeuroSQUID

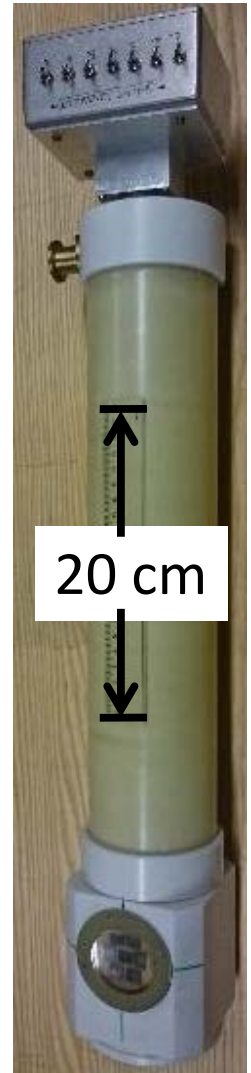
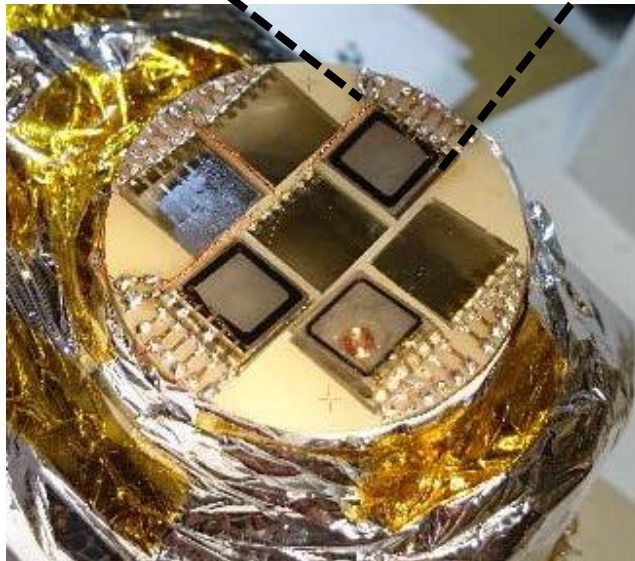
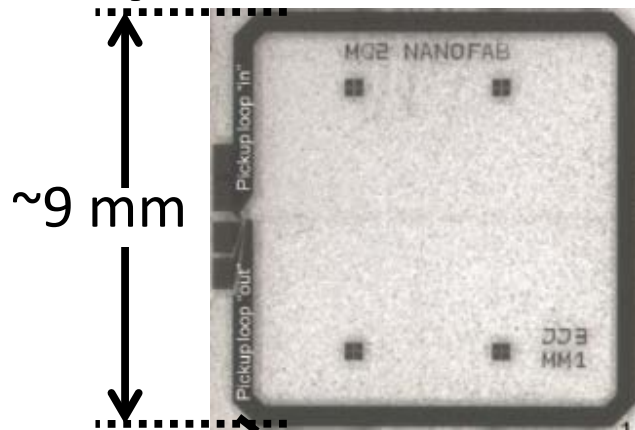
## Cryostat – outer part and inner guts

- Sapphire window on inner LN2 container
- 7 sapphire wedges on d.o. holding SQUIDs
  - Dense, hexagonal pattern (2 mm edge-to-edge)
  - Tilted towards center
- 3 x 3-channel electronics from Magnicon



# NeuroSQUID

## Parts and pieces



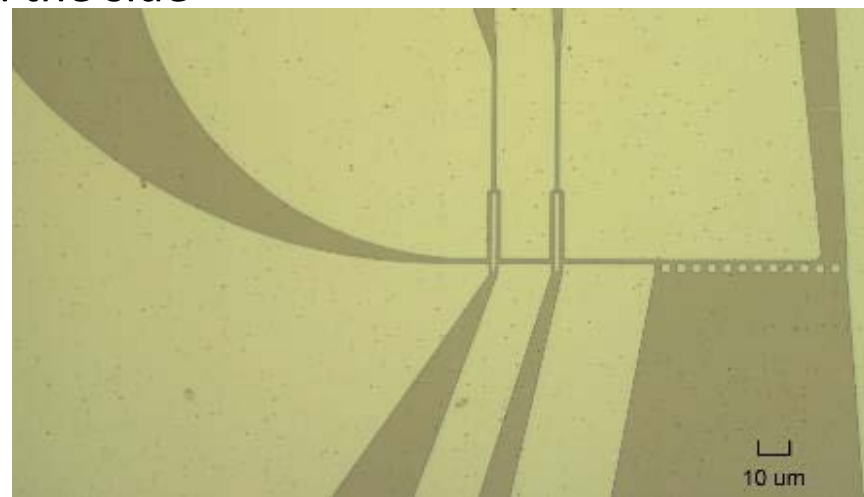
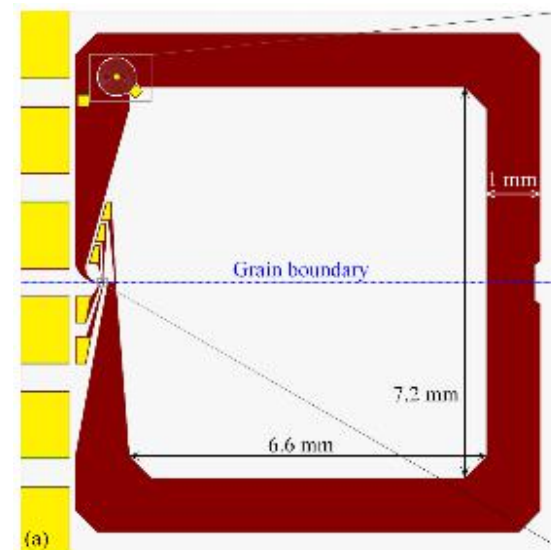




# NeuroSQUID

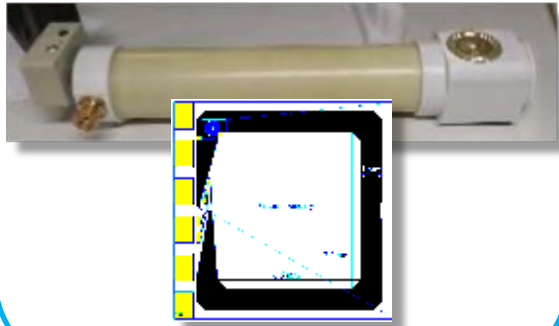
## High- $T_c$ SQUID magnetometer

- Single layer  $\text{YBa}_2\text{Cu}_3\text{O}_{7-x}$  (YBCO) thin film magnetometer with directly coupled pickup loop
- $10 \times 10 \text{ mm}^2$  STO bicrystal substrate
- 2 grain boundary Josephson junction dc SQUIDs per chip
- High  $I_C R_n$  product: 120 – 250  $\mu\text{V}$  at 77 K
- Rounded gold edges to contact from the side

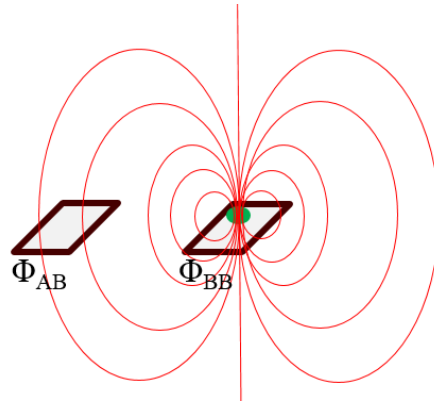


# NeuroSQUID

## Cryostat and sensors



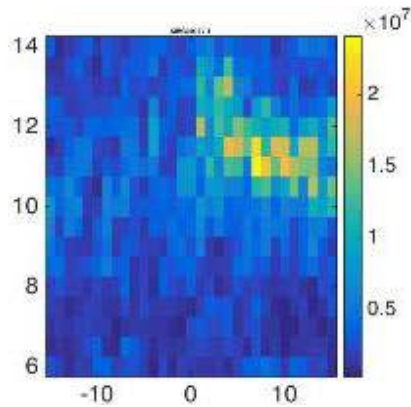
## Crosstalk



## Head phantom measurements



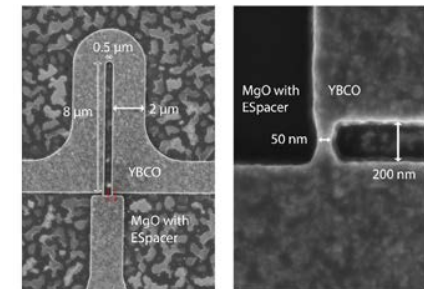
## Preliminary alpha



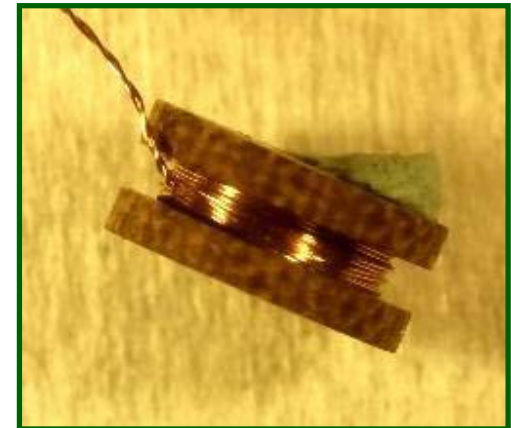
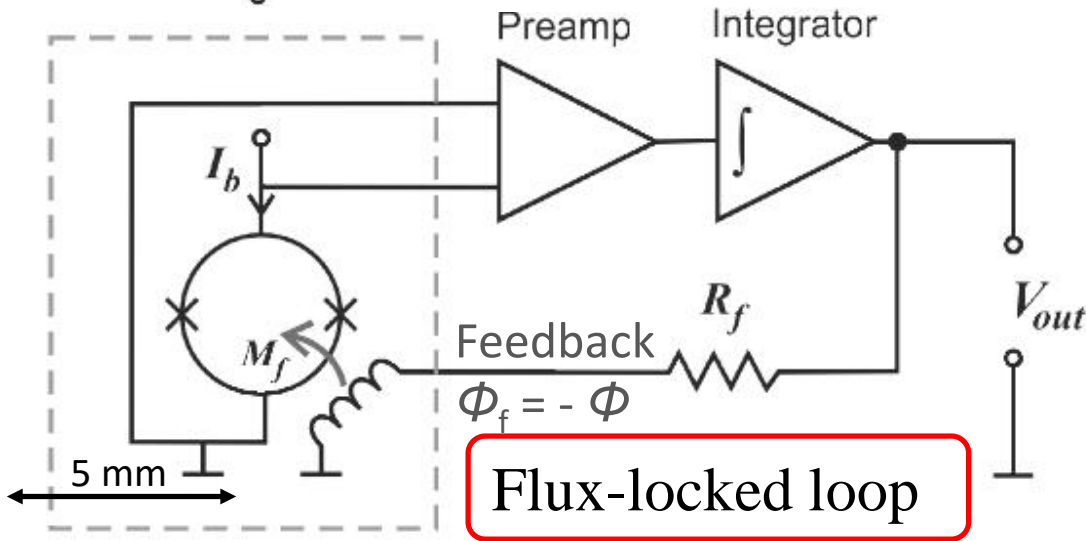
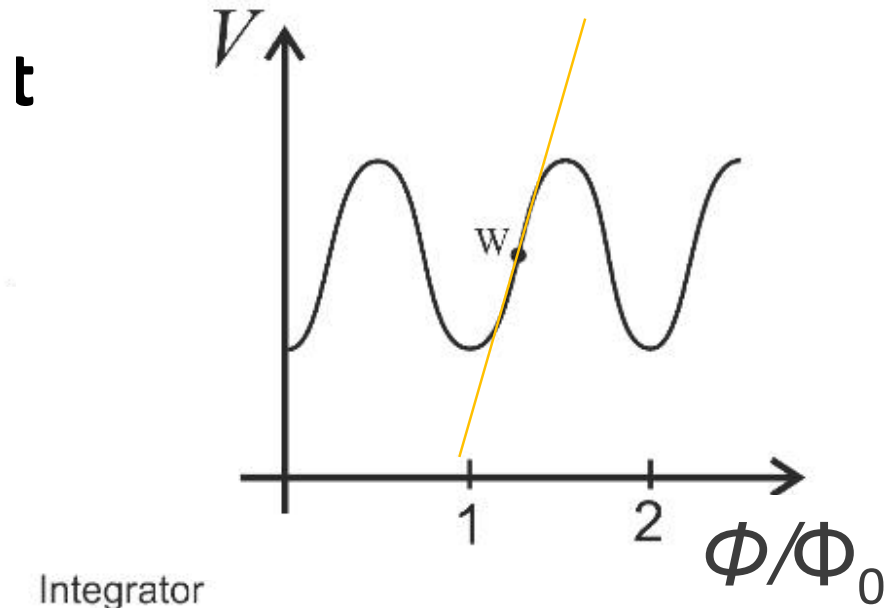
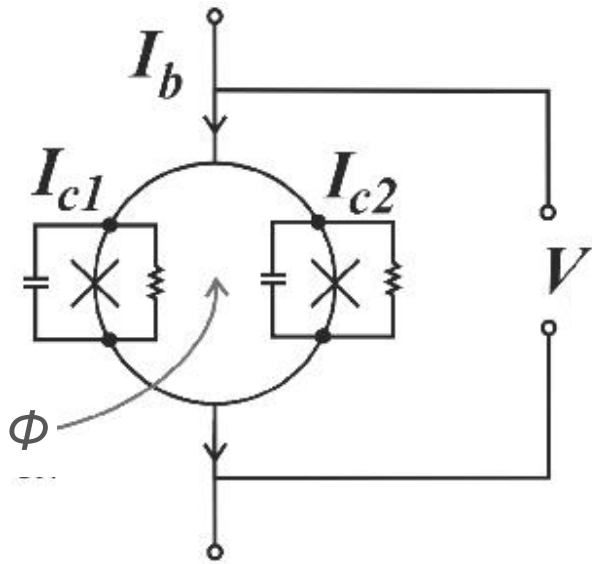
## Next step: Flux transformers



## Next step: Nanowire-based SQUIDs



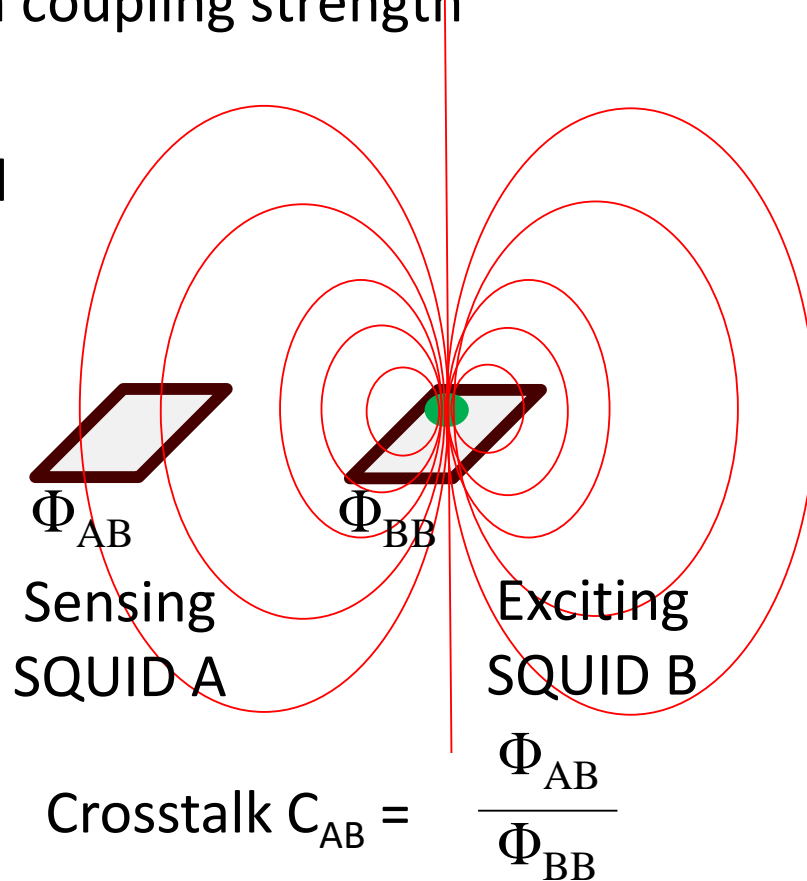
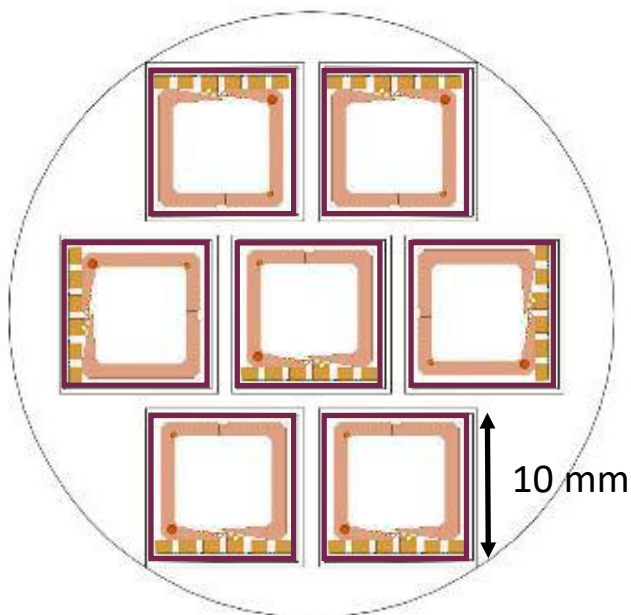
# NeuroSQUID



# NeuroSQUID

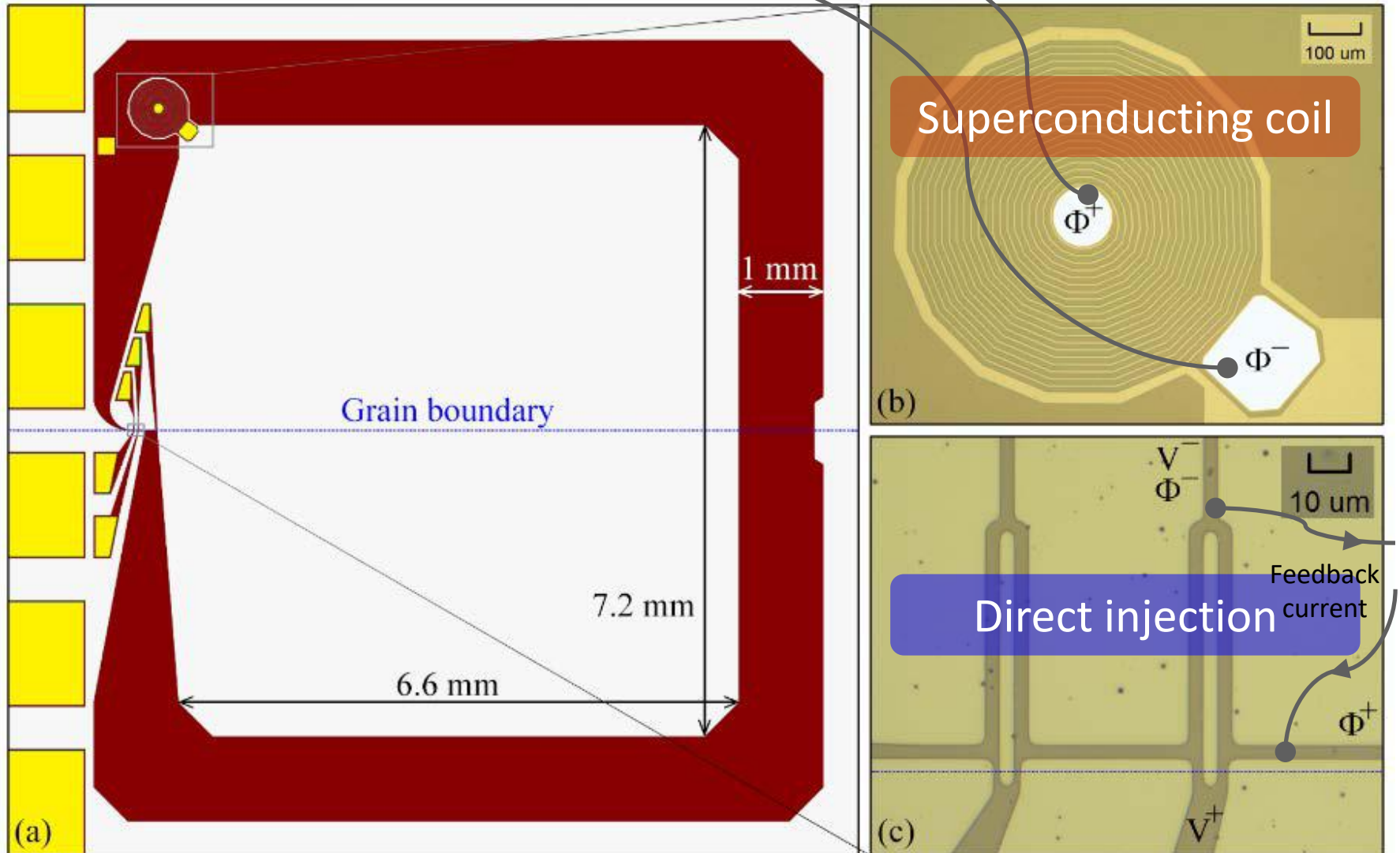
## Criteria for feedback

- On-scalp MEG → minimize standoff distance
- Flux-locked loop → high enough coupling strength
- Low noise
- Low crosstalk → densely packed



# Feedback solutions

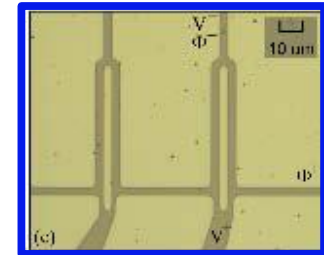
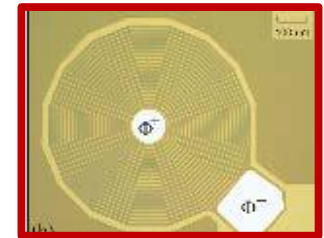
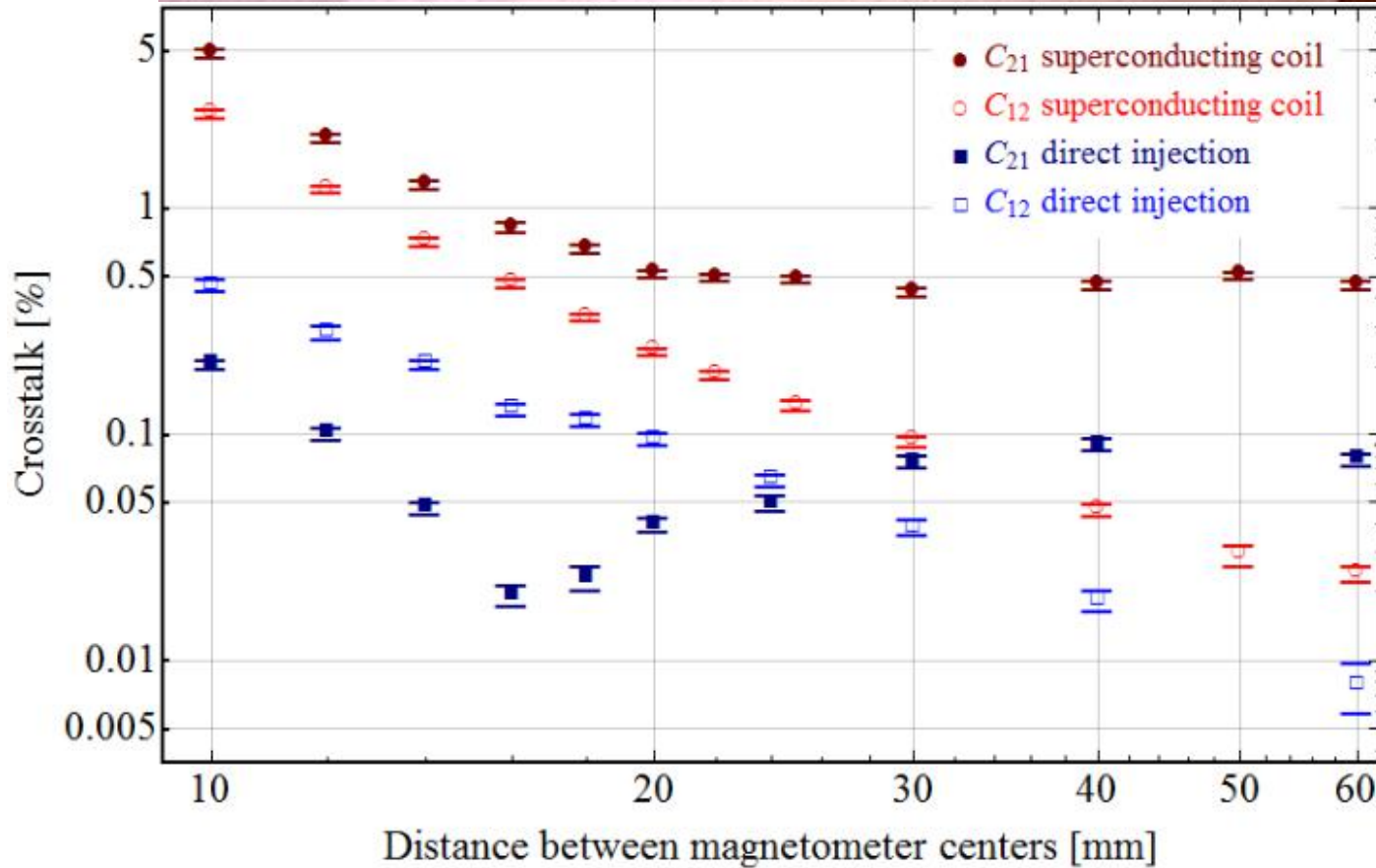
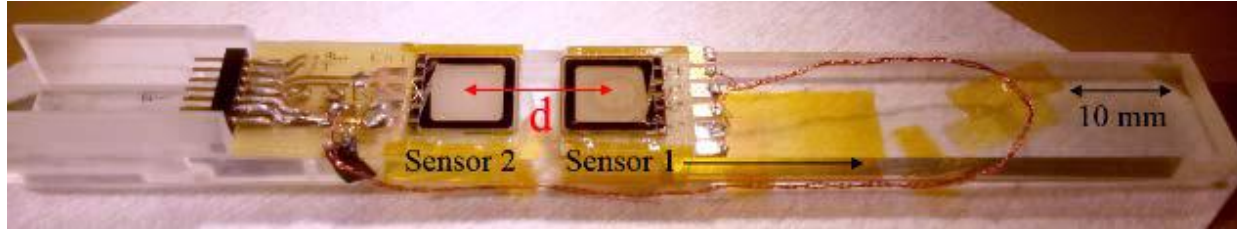
Feedback current



Superconducting coil

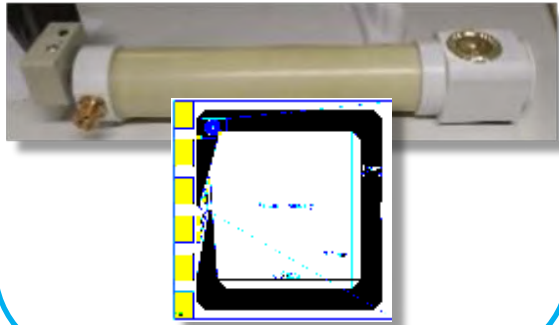
Direct injection

# Crosstalk NeuroSQUID

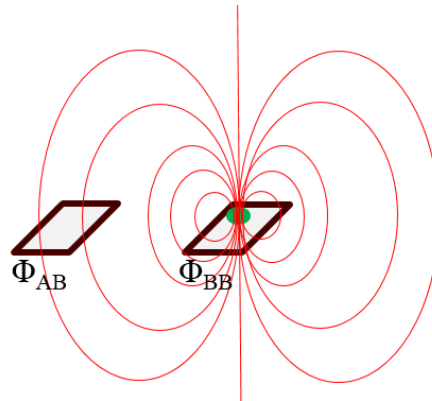


# NeuroSQUID

## Cryostat and sensors



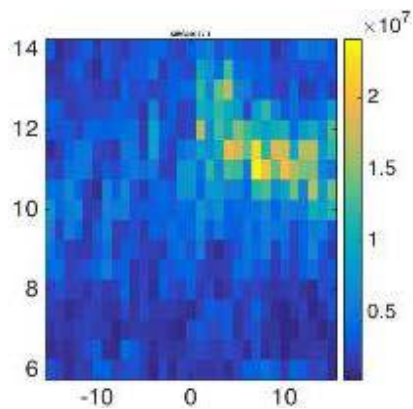
## Crosstalk



## Head phantom measurements



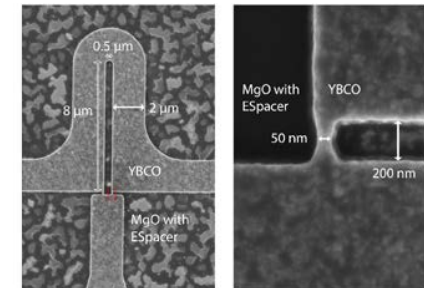
## Preliminary alpha



## Next step: Flux transformers



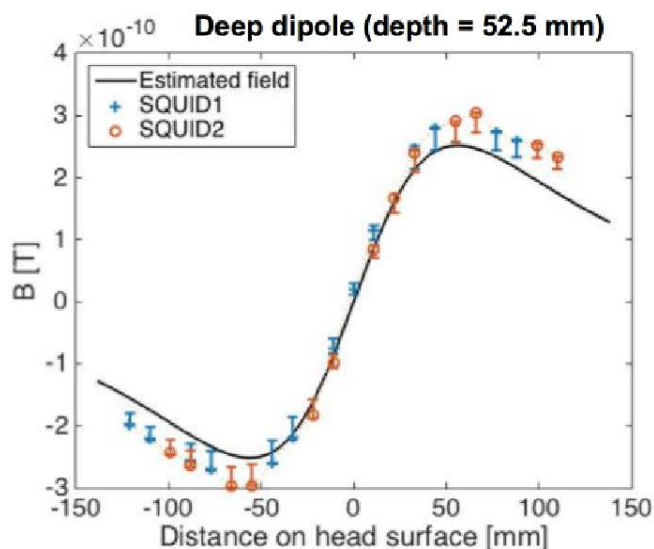
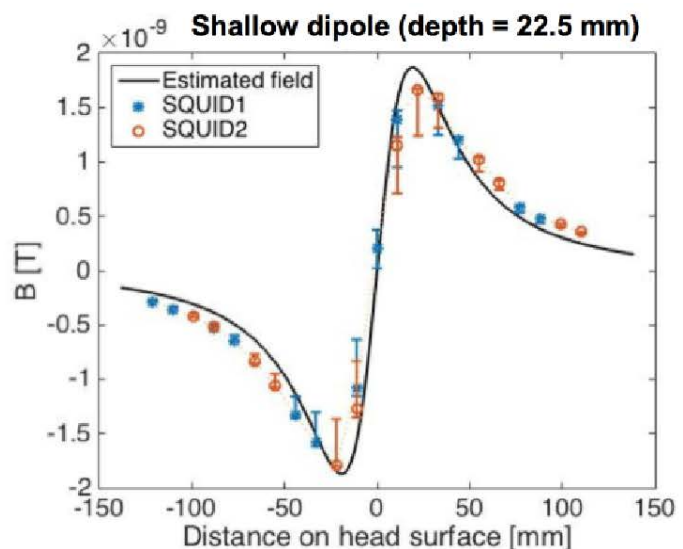
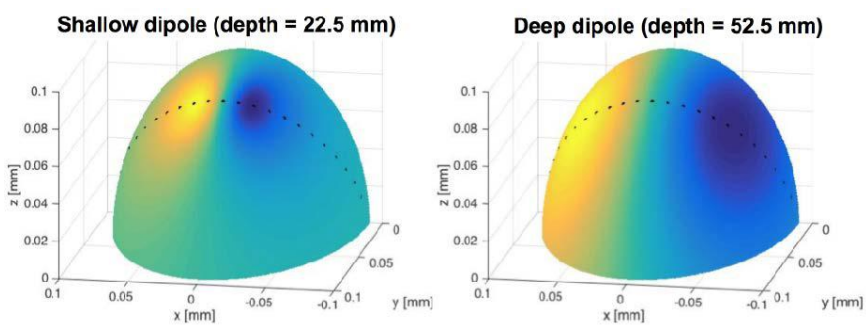
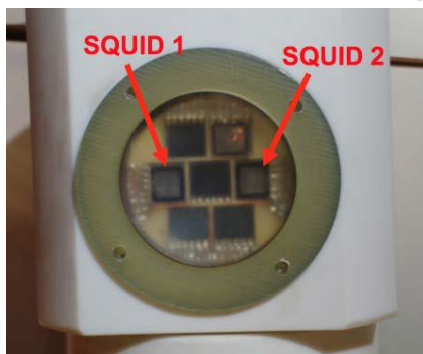
## Next step: Nanowire-based SQUIDs





# NeuroSQUID

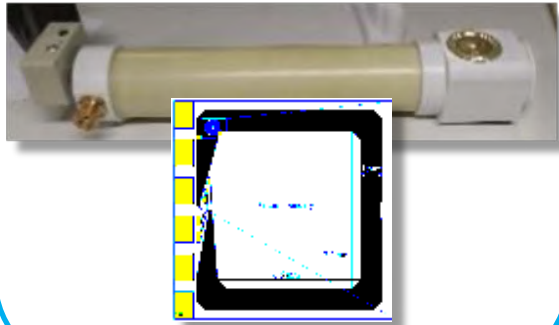
## 2 Channel phantom measurements



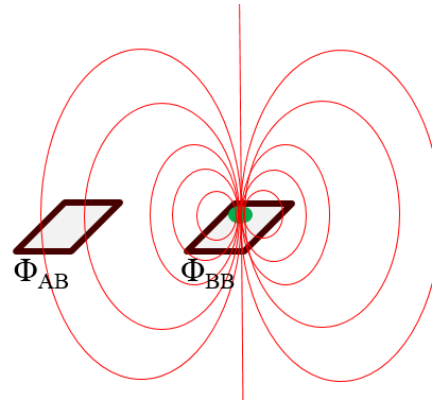


# NeuroSQUID

## Cryostat and sensors



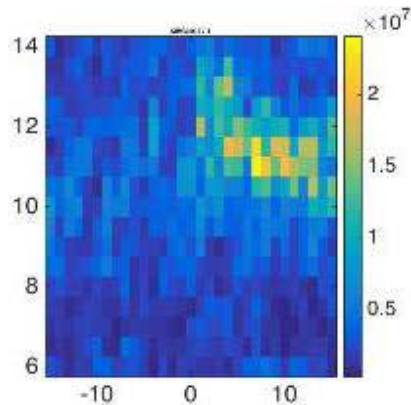
## Crosstalk



## Head phantom measurements



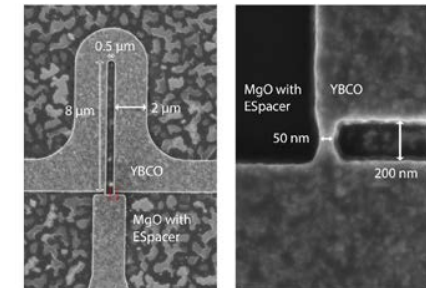
## Preliminary alpha



## Next step: Flux transformers



## Next step: Nanowire-based SQUIDs



# NeuroSQUID

## Preliminary measurements on alpha

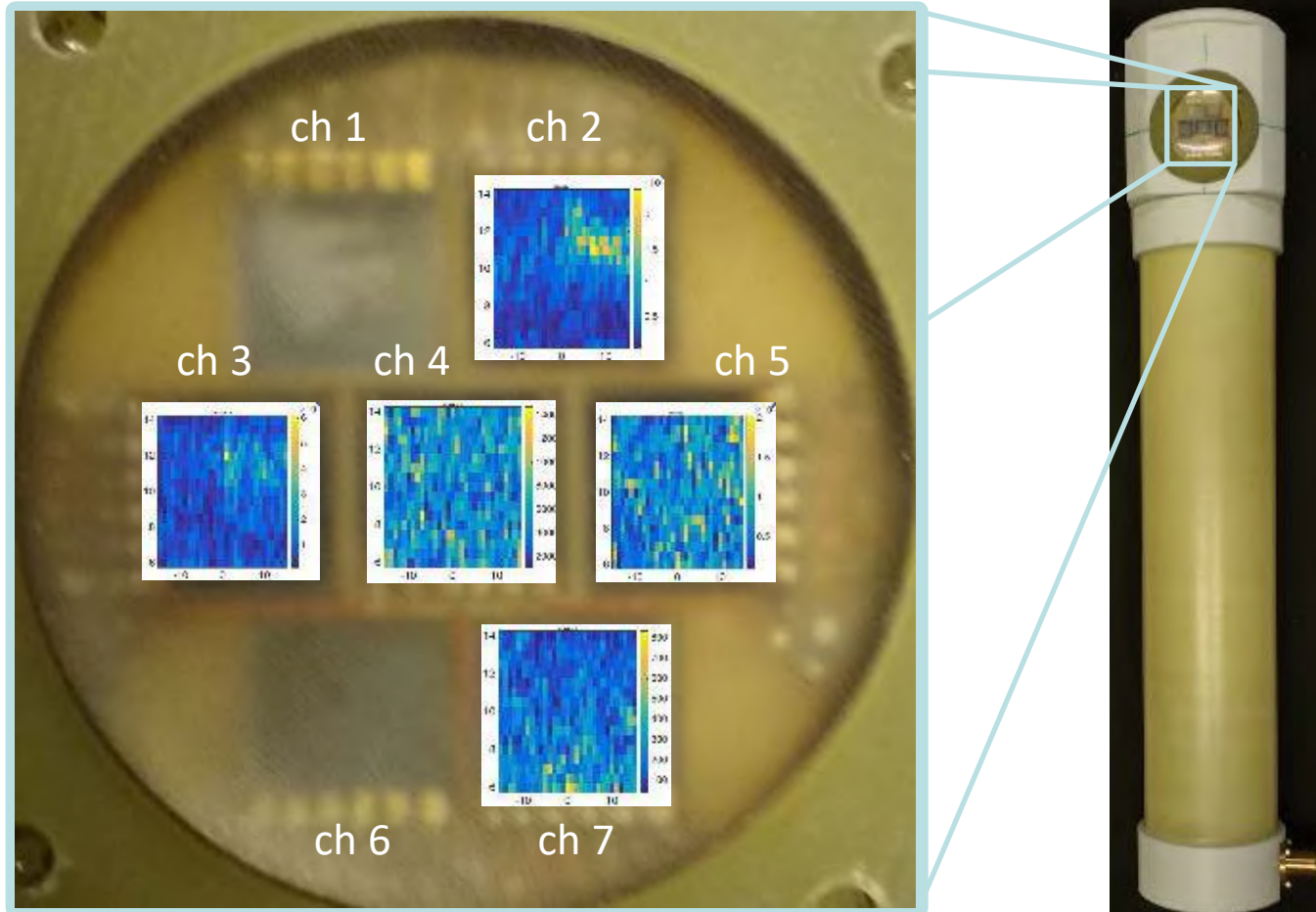


- 5 (7) SQUIDs
- Alpha (8-12 Hz)
- Eyes open – eyes closed
- Time-frequency spectra (using multitapers)
- Average over 5 trials



# NeuroSQUID

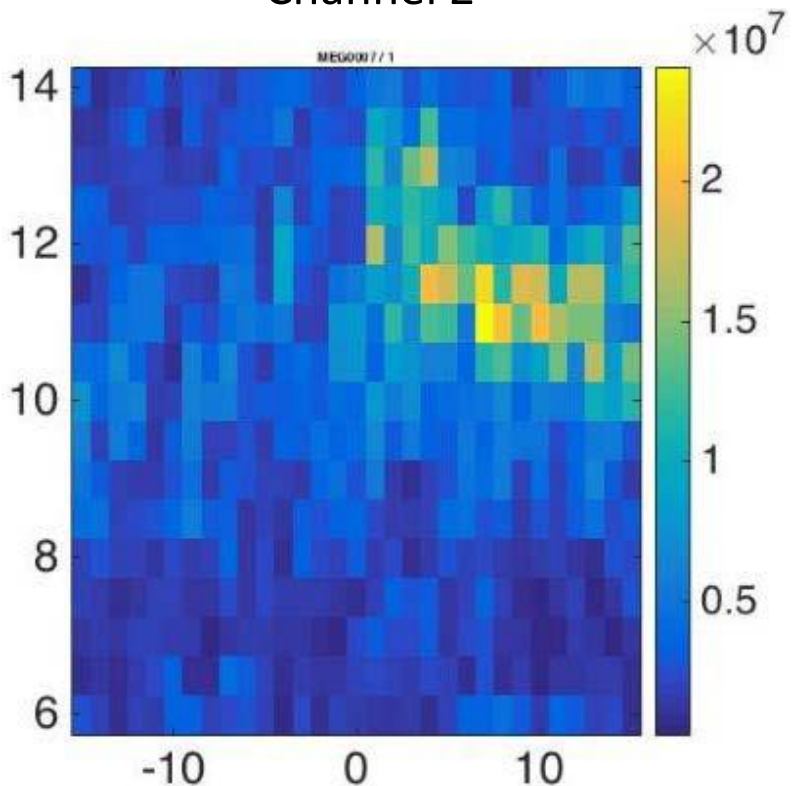
## Preliminary measurements on alpha



# NeuroSQUID

## Preliminary measurements – increase in alpha seen in channel 2 & 3

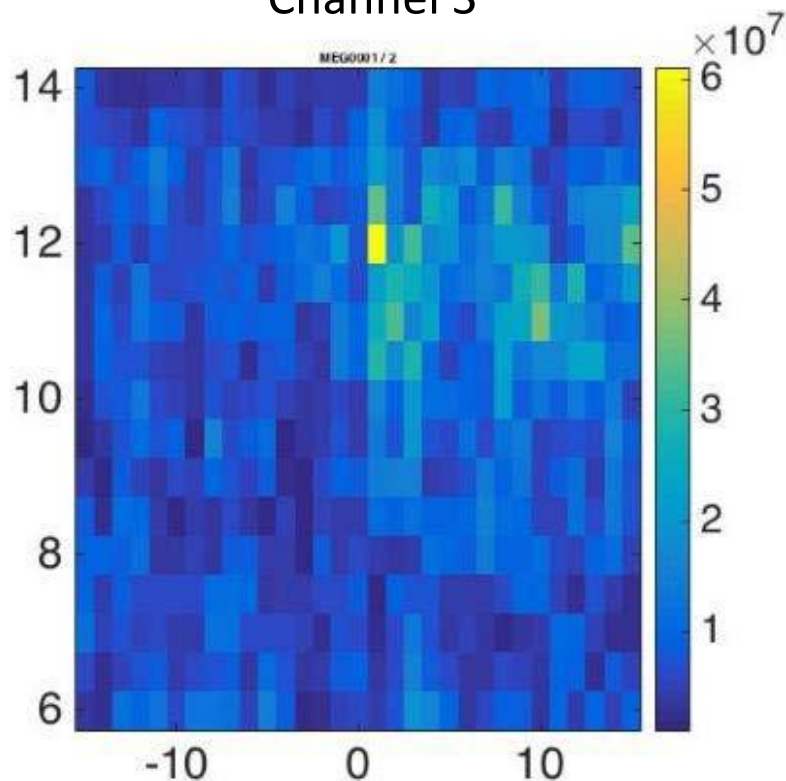
Channel 2



eyes open  
30 seconds

| eyes closed  
30 seconds

Channel 3

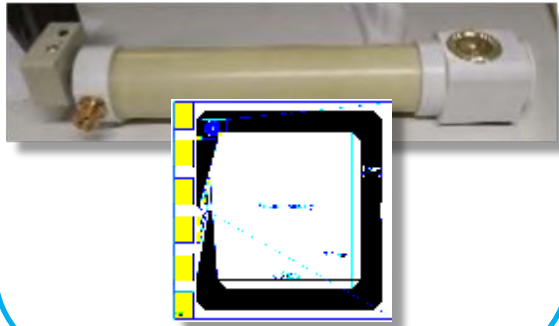


eyes open  
30 seconds

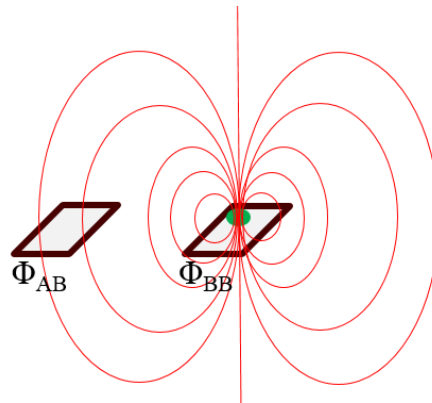
| eyes closed  
30 seconds

# NeuroSQUID

## Cryostat and sensors



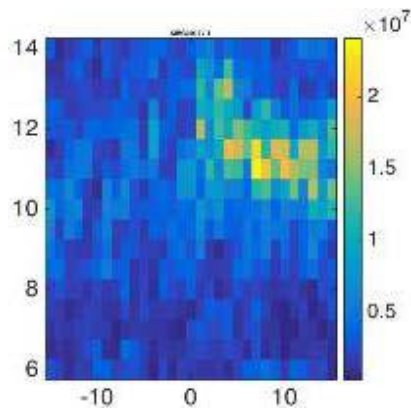
## Crosstalk



## Head phantom measurements



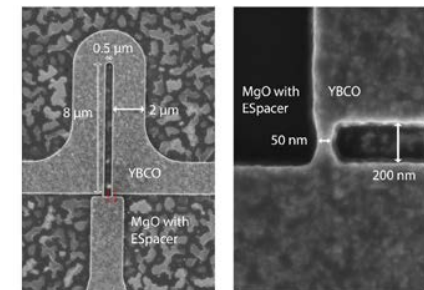
## Preliminary alpha



## Next step: Flux transformers



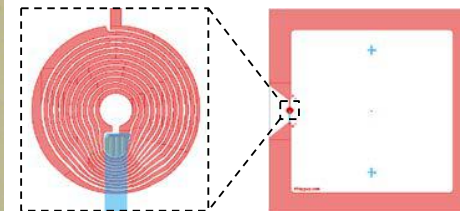
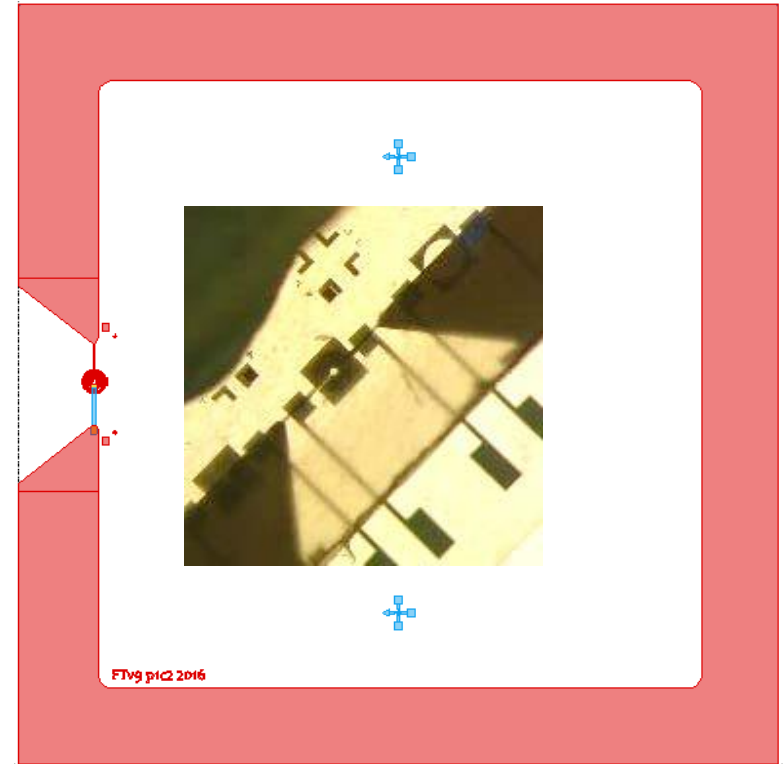
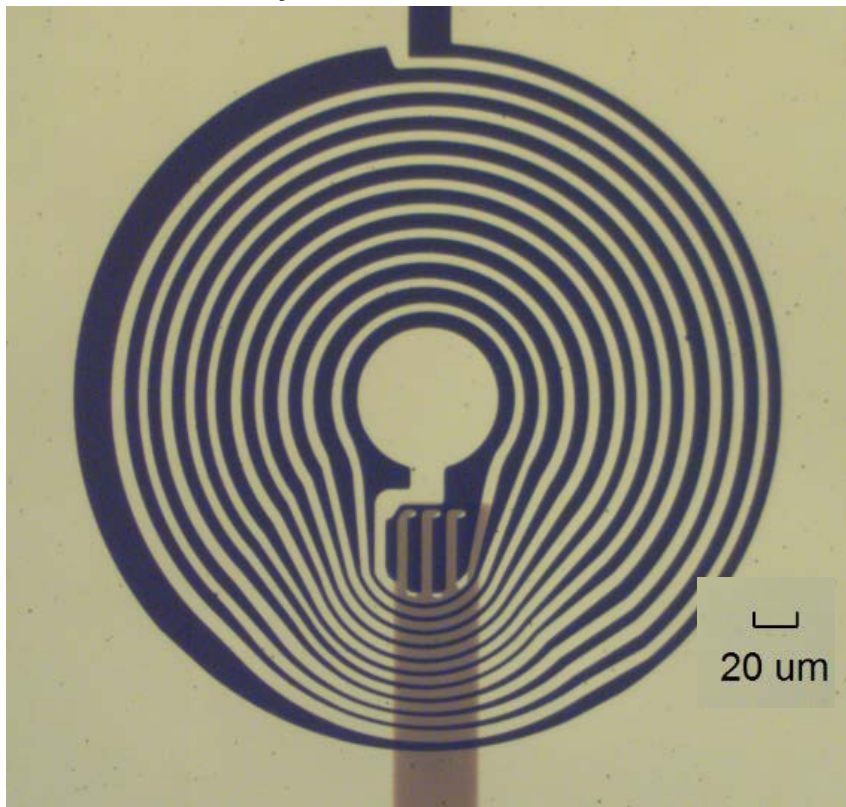
## Next step: Nanowire-based SQUIDs



# NeuroSQUID

## Flux transformers

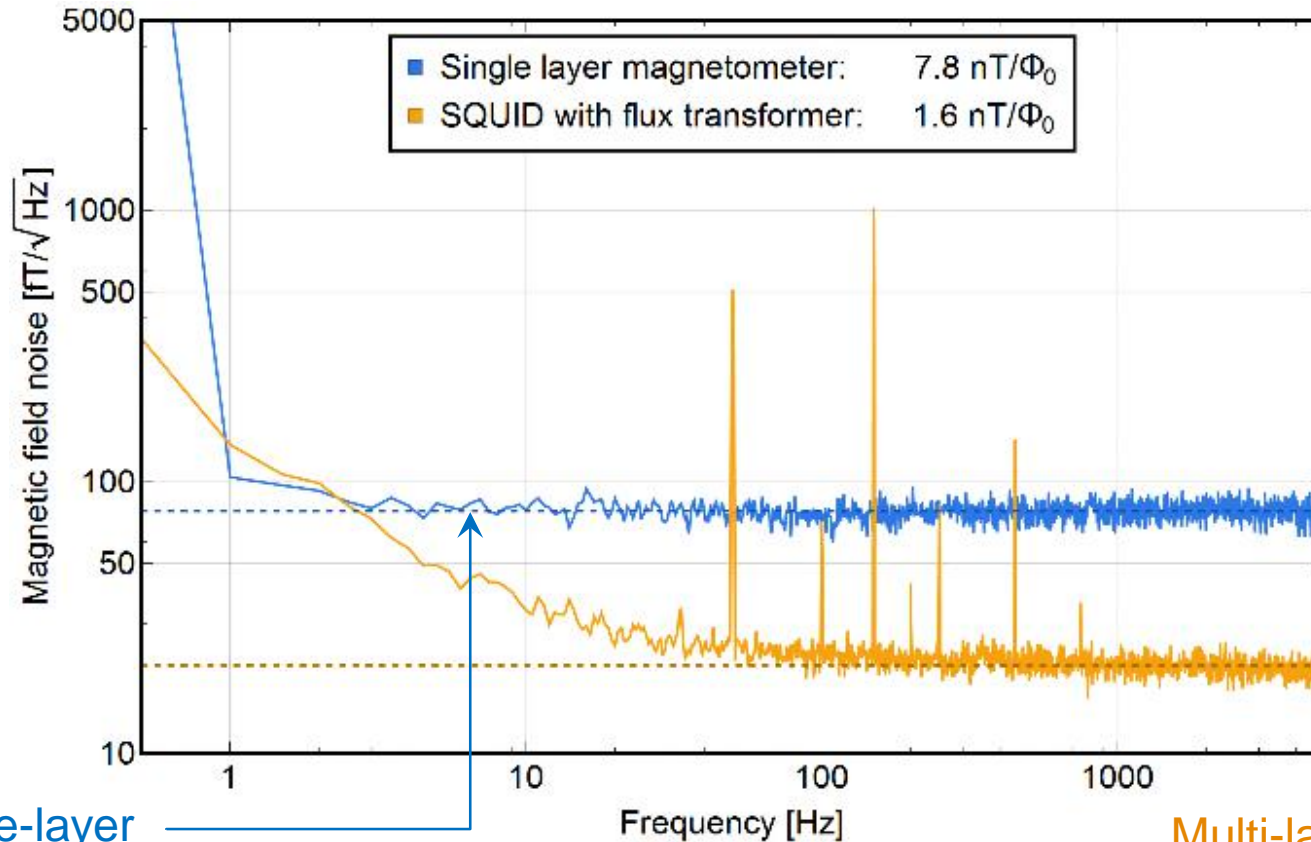
- Increase effective area  $A_{\text{eff}}$
- Multi-layer device



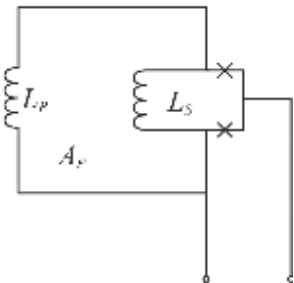
Flip-chip device



# Flux transformers (for flip-chip) NeuroSQUID



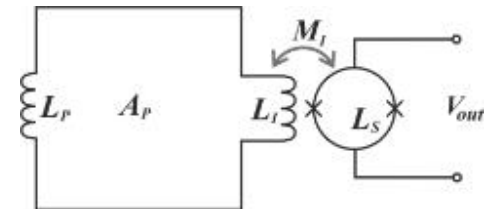
Single-layer



- Easy to fabricate
- Limited effective area / sensitivity

- Better effective area / sensitivity
- Challenging fabrication

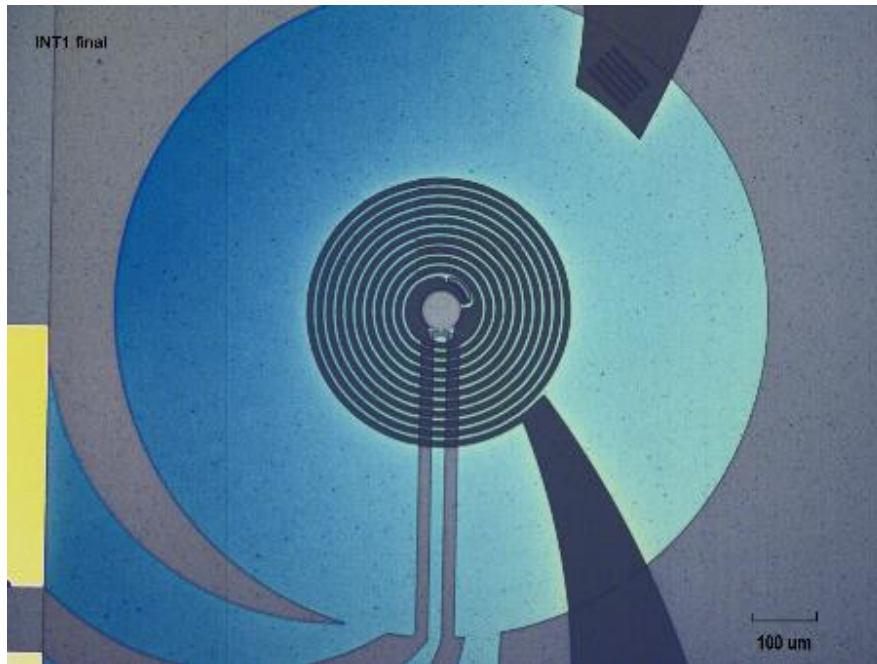
Multi-layer FT flip-chip



# NeuroSQUID

## Integrated flux transformer

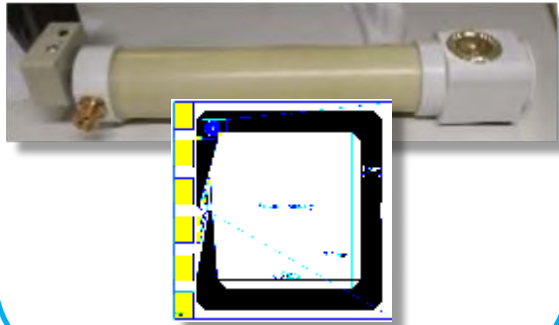
- Single chip
- Increased coupling



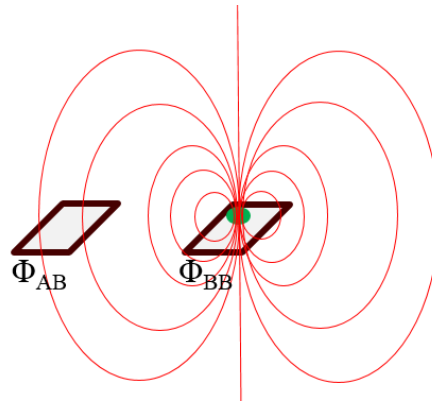


# NeuroSQUID

## Cryostat and sensors



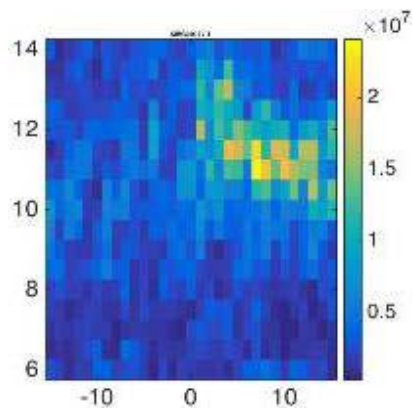
## Crosstalk



## Head phantom measurements



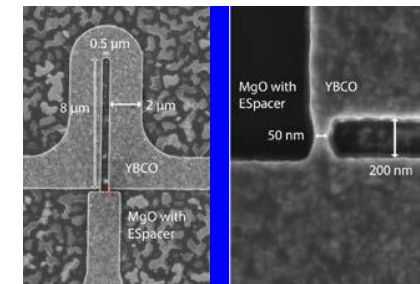
## Preliminary alpha



## Next step: Flux transformers

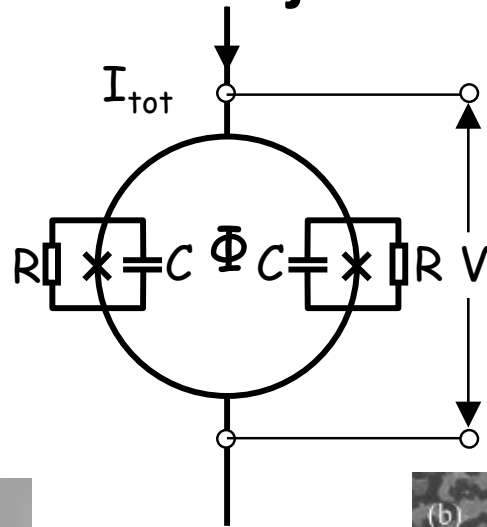


## Next step: Nanowire-based SQUIDs

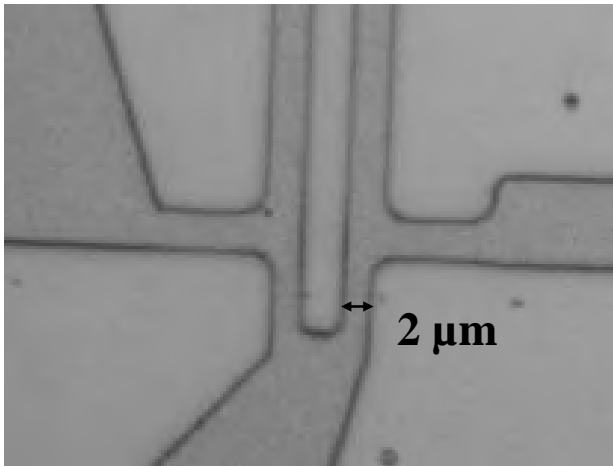


# NeuroSQUID

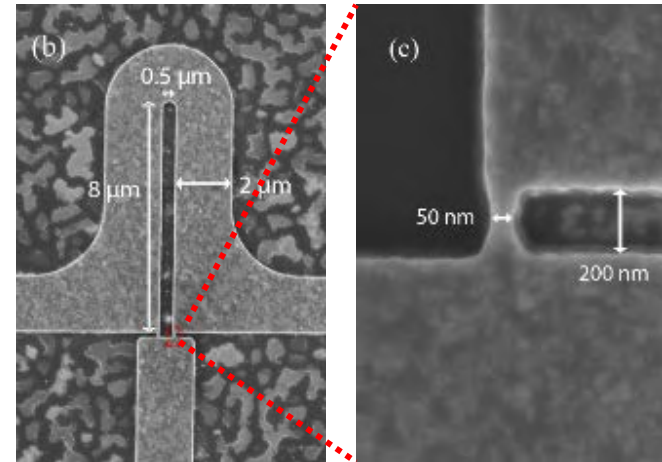
## Moving from bicrystal grain boundary to nanowire junctions



Bicrystal grain boundary junctions

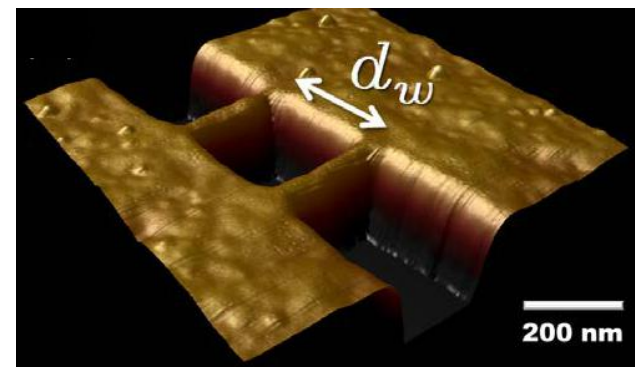
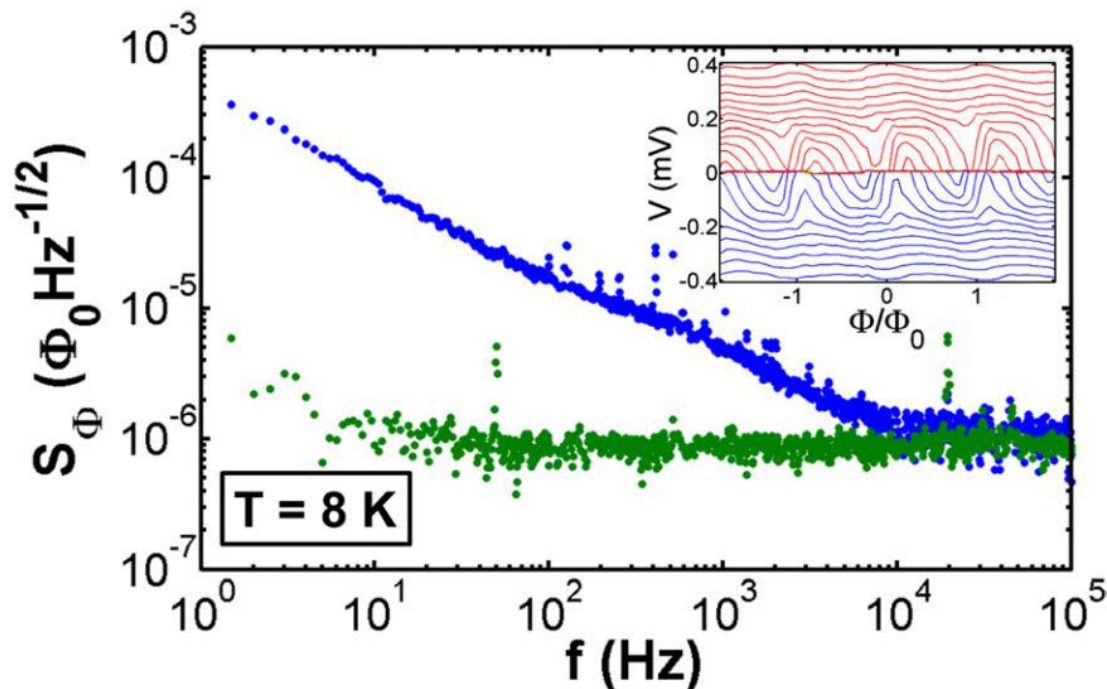


Nanowire junctions



# NeuroSQUID

## Motivation: Previous work\* on high- $T_c$ nano-SQUIDs



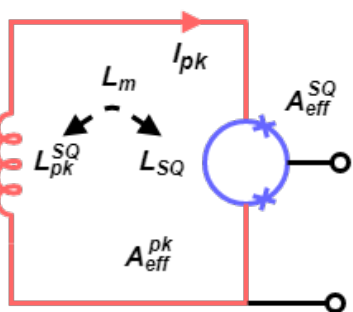
- Low flux noise at 8 K → what about at 77 K?
- Large  $1/f$  noise → what about under bias-reversal condition?
- Small SQUID loop size → can it be used as a magnetometer?
- Scalable junction technology → potential for multi-channel MEG?

\*) R. Arpaia, et al., *Appl. Phys. Lett.*, vol.104, 2014

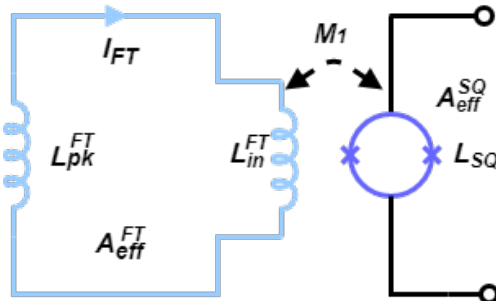
# NeuroSQUID

## Three approaches for coupling

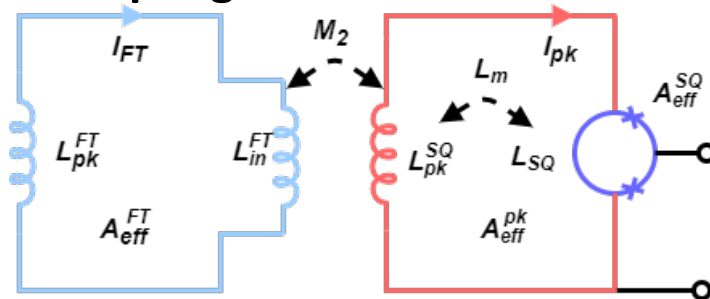
### Approach I



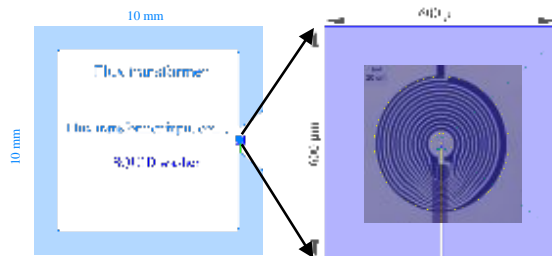
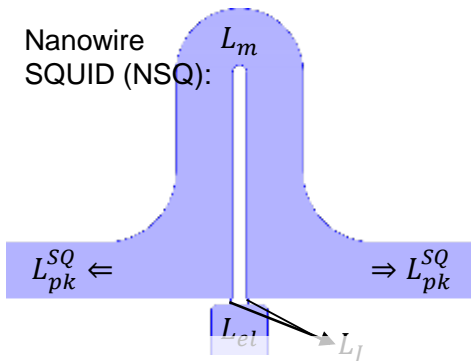
### Approach II: with a flux transformer



### Approach III: A two-level coupling method



Nanowire SQUID (NSQ):



M. Chukharkin et al., IEEE Trans. Appl. Supercond., vol. 23, pp. 1602704, 2013



$$A_{eff} = 0.09 \text{ mm}^2$$

$$S_{\phi}^{1/2} = 55 \mu\Phi_0/\sqrt{\text{Hz}}$$

$$S_B^{1/2} = \mathbf{1200 \text{ fT}/\sqrt{\text{Hz}}}$$

$$A_{eff} = 0.16 \text{ mm}^2$$

$$S_{\phi}^{1/2} = 35 \mu\Phi_0/\sqrt{\text{Hz}}$$

$$S_B^{1/2} = \mathbf{480 \text{ fT}/\sqrt{\text{Hz}}}$$

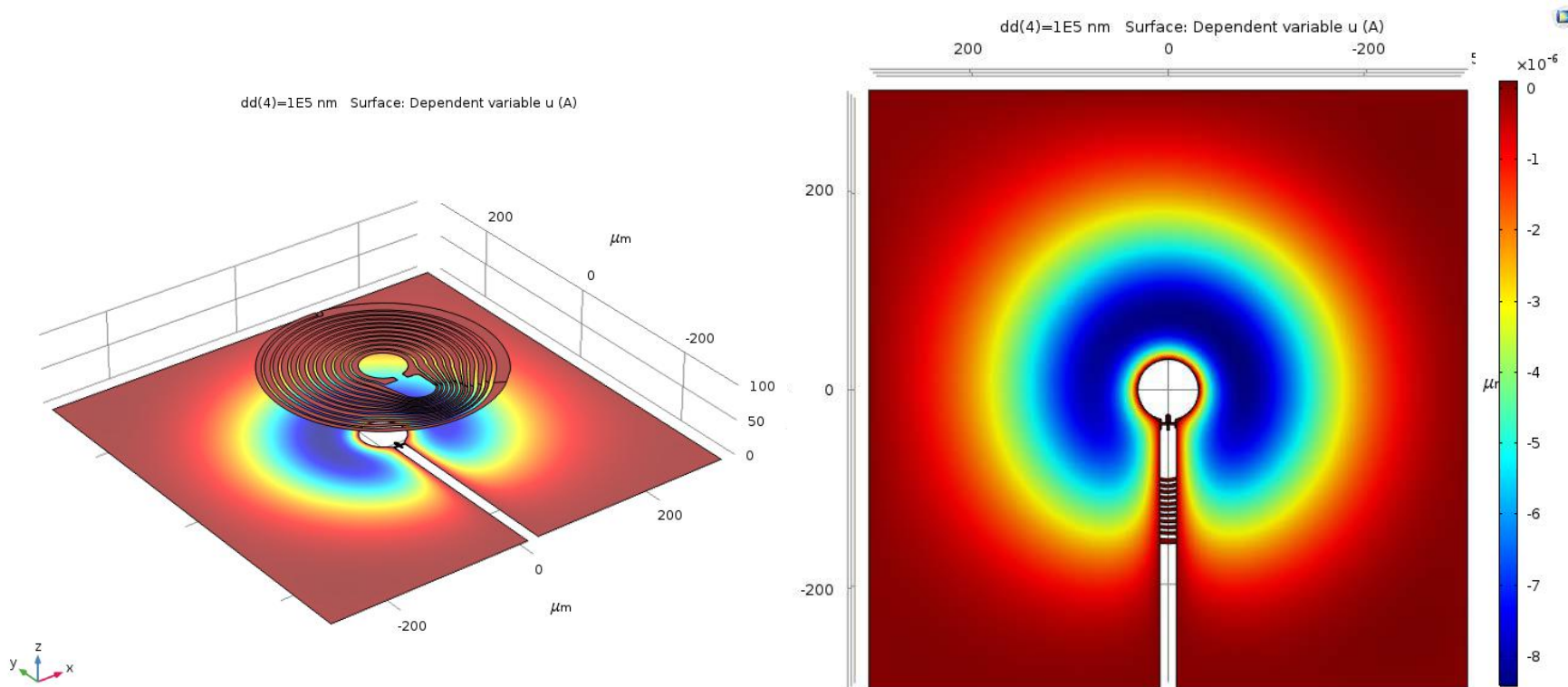
$$A_{eff} = 0.46 \text{ mm}^2$$

$$S_{\phi}^{1/2} = 55 \mu\Phi_0/\sqrt{\text{Hz}}$$

$$S_B^{1/2} = \mathbf{240 \text{ fT}/\sqrt{\text{Hz}}}$$

# NeuroSQUID

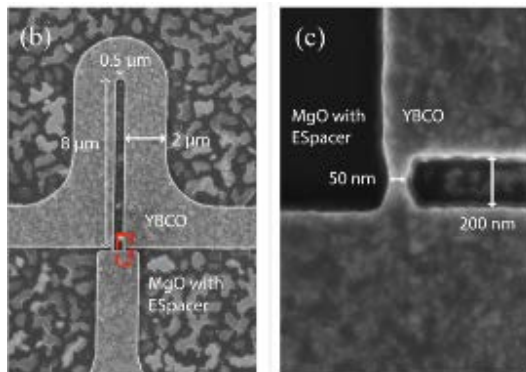
## Simulation toolbox for numerically calculating the inductances and coupling



- Software: AutoCAD and COMSOL Multiphysics
- Principle: Solving London and Maxwell Eqs with the concept of stream function

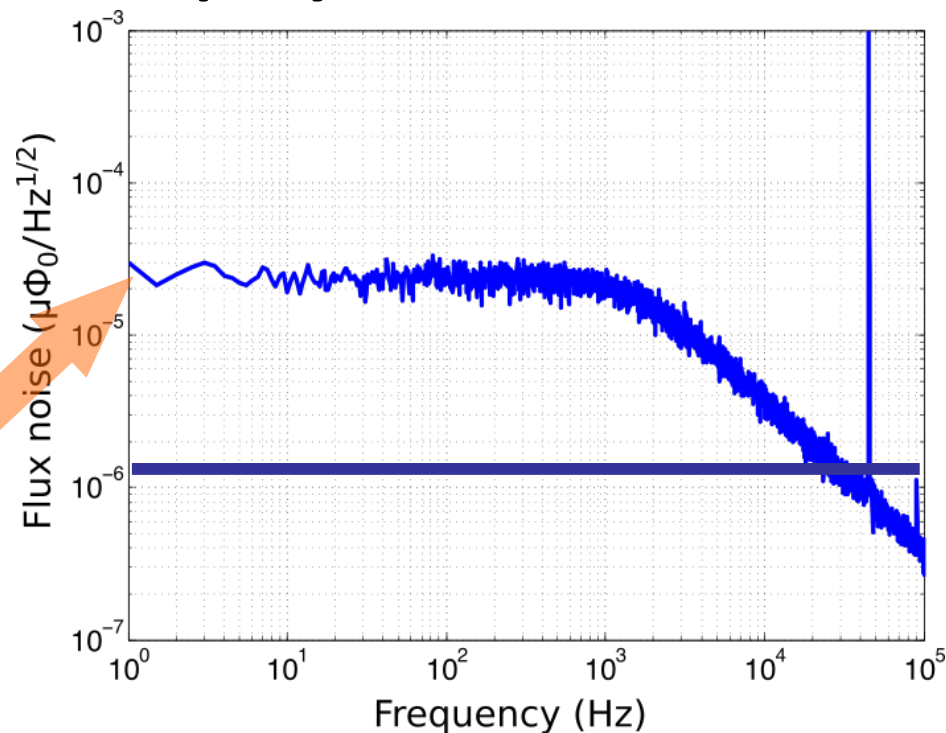
# NeuroSQUID

## Noise at 77 K without Au top layer



50 nm YBCO:

- no Au capping
- no pick up loop
- $V_{\phi} \sim 15 \mu\text{V}/\phi_0$
- Amp:  $S_v^{1/2} \sim 0.4 \text{ nV}/\text{Hz}^{1/2}$



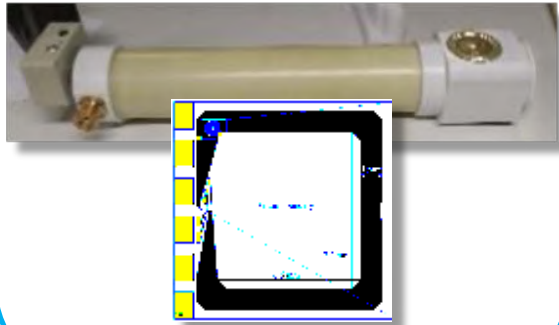
Expected field noise taking achieved effective area  $A_{\text{eff}} \sim 0.1 \text{ mm}^2$ :  $S_{\phi}^{1/2} \sim 500 \text{ fT}/\text{Hz}^{1/2}$

For HTS MEG applications:  $S_{\phi}^{1/2} < 50 \text{ fT}/\text{Hz}^{1/2}$  needed

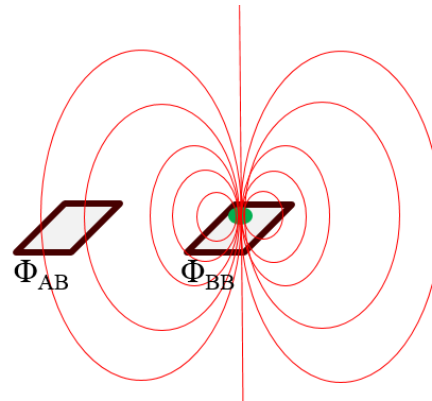
→ SQUID electronics with lower input noise (Cryoton)

# NeuroSQUID

## Cryostat and sensors



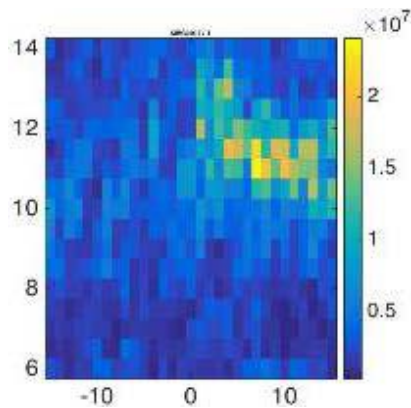
## Crosstalk



## Head phantom measurements



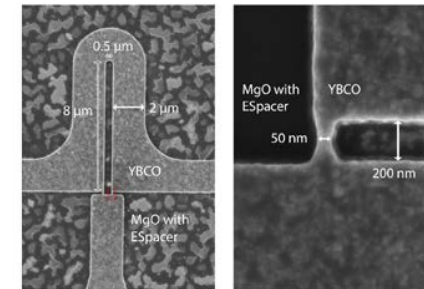
## Preliminary alpha



## Next step: Flux transformers



## Next step: Nanowire-based SQUIDs



# CONCLUSIONS

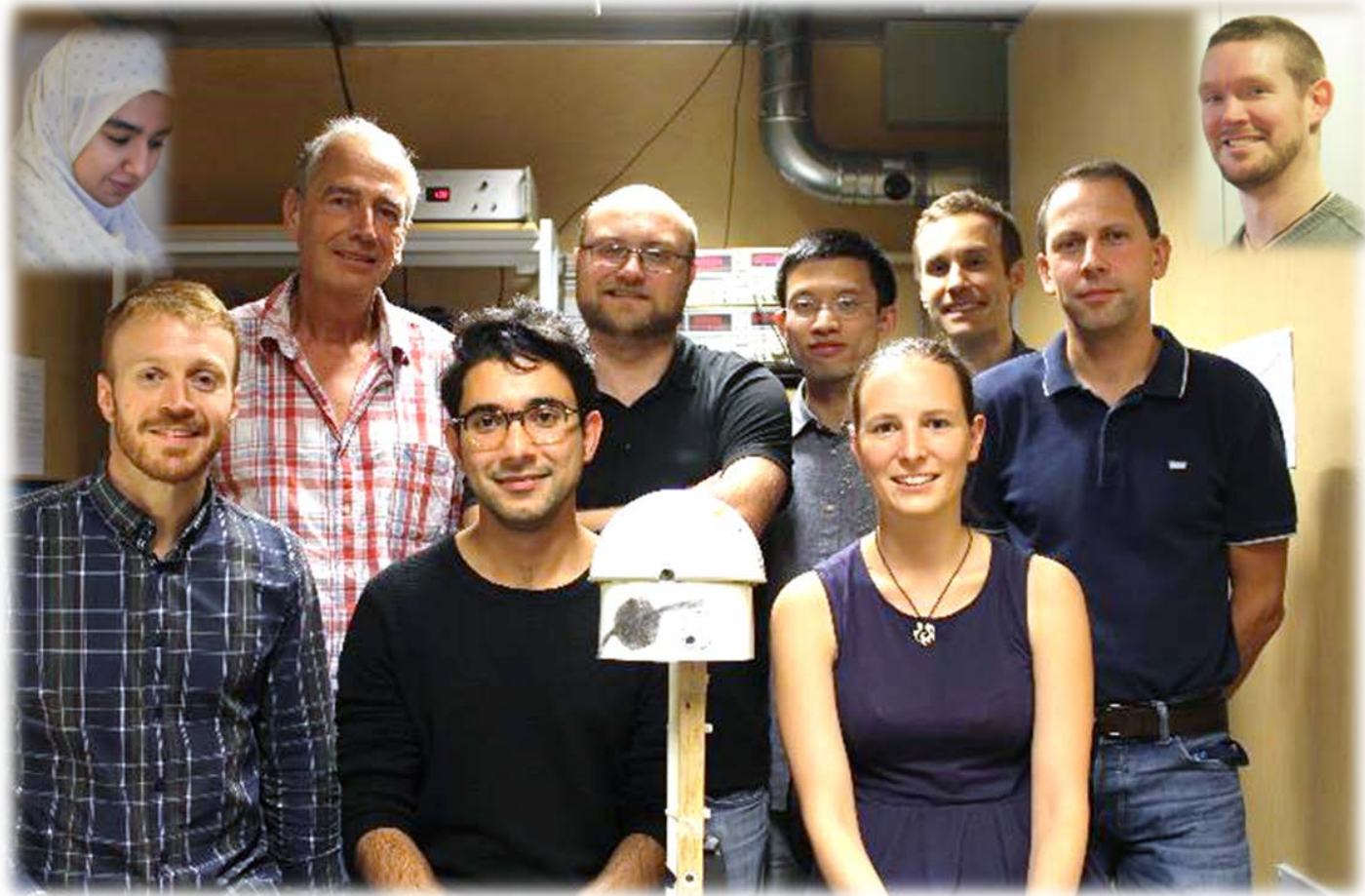
- We still have to struggle a bit to get further down the road...

- HTS vs. LTS MEG
  - Benchmarking has been made with phantoms and humans
  - HTS MEG reveals strange theta at occipital region
  - HTS MEG shows larger than expected signals for shallow sources
  - HTS MEG shows more complex signals
- A 7-channel high-Tc SQUID-based MEG system is being built:
  - Crosstalk between two channels caused by feedback has been studied
  - Phantom and human subjects measured
  - System level benchmarking (source localization) to be carried out
- Low-noise flux-transformers for
  - Flip-chip and possibly integrated devices
- To improve the sensitivity of nanowire-based high-Tc SQUID:
  - Thicker washer in Ketchen-type coupling (coupling coeff.  $k$ : 0.05  $\rightarrow$  0.7)
  - Integrated devices (smaller separation)
  - Projected sensitivity 10 fT/√Hz for Ketchen-type coupling





# The Chalmers SQUID group



*Knut och Alice  
Wallenbergs  
Stiftelse*

**MedTech West**



**GÖTEBORGS  
UNIVERSITET**



**CHALMERS**

**MC2**  
Microtechnology and Nanoscience



Anders Hedström



CHNOLOG  
Göran Pegenius<sup>d</sup>

Fredrik Öisjön<sup>b</sup>



Dag Winkler<sup>b</sup>



Mikael Elam<sup>a,d</sup>



Bushra Riaz<sup>a</sup>

Minshu Xie<sup>b</sup>



Maxim Chukharkin<sup>b,c</sup>



Alexei Kalabukhov<sup>b,c</sup>

Our SQUIDS



GÖTEBORGS UNIVERSITET



CHALMERS



MedTech West

Daniel Lundqvist

Martin Ingvar

Stephen Whitmarsh

Oct 2013

Veikko Jousmäki

Robert Oostenveld

Minshu Xie

Matti Hämäläinen

Lau Møller Andersen

Alexei Kalabukhov

Emily Ruzich

Sara Woxlin

Fanny Lachat

Silvia Ruffieux

Christoph Pfeiffer

Dec 2015



The National Facility for  
Magnetoencephalography

The scientific aim of the NatMEG unit is to establish a national core-facility for MEG within the Swedish Biomedicine Network in order to strengthen the international competitiveness of Swedish Cognitive Neuroscience. The method has not been available in Sweden previously so that especially the time-resolution of the MEG method combined with its localization power provides an additional dimension for functional brain research for all groups that already work with fMRI.



Thanks!

¿QUESTIONS?

